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<p>(21) International Application Number: PCT/US97/12544 (22) International Filing Date: 3 July 1997 (03.07.97) (30) Priority Data: 08/676,867 3 July 1996 (03.07.96) US (60) Parent Application or Grant (63) Related by Continuation US Not furnished (CIP) Filed on Not furnished (71) Applicant (for all designated States except US): UNIVERSITY OF PITTSBURGH [US/US]; 911 William Pitt Union, Pitts- burgh, PA 15260 (US). (72) Inventors; and (75) Inventors/Applicants (for US only): HUANG, Leaf [US/US]; 2468 Matterhorn Drive, Wexford, PA 15090 (US). HARA, Toshifumi [JP/JP]; 3-10-3, Jindaijimotomachi, Chofu-city, Tokyo 182 (JP). (74) Agents: SMITH, Stephen, R. et al.; Morgan & Finnegan, L.L.P., 345 Park Avenue, New York, NY 10154 (US).</p>	<p>(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, GH, HU, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, US, UZ, VN, YU, ZW, ARIPO patent (GH, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).</p> <p>Published With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</p>	
<p>(54) Title: EMULSION FORMULATIONS FOR HYDROPHILIC ACTIVE AGENTS</p> <div data-bbox="669 1171 1091 1558" data-label="Image"> </div> <div data-bbox="565 1570 1156 1696" data-label="Text"> <p>  : egg PC  : lyso PC  : oil  : TC-Chol  : DNA </p> </div> <p>(57) Abstract</p> <p>This invention discloses emulsion formulations comprising an aqueous carrier and the following components: triglyceride, cholesterol, phospholipid, at least one charged lipid, at least one hydrophilic biologically active molecule and, optionally, cholesteryl ester, and/or apoprotein; methods of preparing these emulsions; and the use of these emulsions as vehicles for the delivery of hydrophilic biologically active molecules to cells.</p>		

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EMULSION FORMULATIONS FOR HYDROPHILIC ACTIVE AGENTS

5 This application is a continuation-in-part application of U.S. Serial No. 08/676,867 filed July 3, 1997, the contents of which are hereby incorporated by reference.

Field of Invention

10 This invention relates to emulsions and their use as delivery vehicles for biologically active molecules. In particular, the invention relates to emulsion formulations comprising an aqueous carrier and the following components: triglyceride, cholesterol, phospholipid, charged lipid, hydrophilic biologically
15 active molecule and optionally, cholesteryl ester, and/or apoprotein(s); to methods of preparing these emulsions; and to their uses as vehicles for the delivery of hydrophilic biologically active molecules to cells.

Background of Invention

20 The field of selective delivery of biologically active molecules to specific cellular targets is rapidly advancing. Among the various systems that have been studied for their ability to deliver bioactive molecules
25 to cells, lipoproteins, which form naturally occurring biological emulsions, are considered attractive as delivery vehicles for a number of reasons: 1) as endogenous carriers of cholesterol and other lipids in the blood circulation, they are not immunogenic and escape
30 recognition by the reticuloendothelial system; 2) physicochemical characterization of drug-loaded lipoproteins indicates that particles with the same physicochemical properties as the native lipoproteins can be obtained; 3) lipoproteins are removed from the
35 circulation by specific receptors that recognize their

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apoproteins or, they may be directed to nonlipoprotein receptors by chemical modification of their apoproteins (see, for example, Bijsterbosch, M.K. and van Berkel, T.J.C. (1990) Adv. Drug Delivery Revs., 5:231-251); 4) lipoproteins are physically stable due to their compact, neutral, apolar core; 5) the apolar core of lipoproteins provides an ideal domain for lipophilic molecules since molecules that are transported in the core of the lipoprotein are protected from the environment during transportation and the environment is protected from the molecule; and 6) lipoproteins can be synthesized from commercially available lipids and isolated apoproteins.

Examples of the use of lipoproteins as delivery vehicles for bioactive molecules include U.S. Patent Numbers 4,868,158 and 5,324,821 which refer to the preparation of lipoproteins modified by incorporation of a lipophilic active substance into their apolar core. However, since many of the biologically active molecules used for treatment and/or prevention of diseases are too hydrophilic for incorporation into the apolar core of lipoproteins, investigators have attempted to find methods which would permit the incorporation of hydrophilic molecules into lipoproteins.

One approach that has been utilized is to couple hydrophilic molecules to hydrophobic anchors in order to render the hydrophilic molecule more lipophilic. For example, van Berkel has reported the synthesis of a dioleoyl derivative of the anti-viral nucleoside analogue iododeoxyuridine and its incorporation into either high density lipoproteins (HDL) (Bijsterbosch, M.K. et al. (1994) Biochemistry, 33:14073-14080) or chylomicrons (Rensen, P.C.N. et al. (1995) Nature Medicine, 1:221-225). Unfortunately, the use of conjugation to facilitate incorporation of hydrophilic molecules into lipoproteins has a number of potential drawbacks: 1) since the

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0 conjugated molecules are typically incorporated into a
lipid or a protein residue on the surface of the
lipoproteins, the conjugated molecule may interfere with
the interaction of the apoprotein of the lipoprotein and
its receptor; 2) such surface-modified particles may show
5 a greater tendency to aggregate due to a potential loss of
surface charge; 3) attachment of bioactive molecules to
the surface of lipoproteins exposes the molecules to the
environment and vice versa; 4) "derivatization" of
hydrophilic molecules by conjugation to hydrophobic
10 anchors may affect the biological activity of the
hydrophilic molecule; and 5) such a "conjugation" approach
is impractical for rendering larger molecular weight
hydrophilic molecules hydrophobic enough to be
incorporated into the apolar core of the lipoproteins.

15

Summary of the Invention

The present invention relates to emulsion
formulations designed to mimic native (i.e. naturally
occurring) lipoprotein emulsions in vivo.

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The emulsion formulations of the invention
comprise an aqueous carrier and the following components:
triglyceride, cholesterol, phospholipid, at least one
charged lipid, at least one hydrophilic biologically
active molecule, and optionally, protein(s), and/or
25 cholesteryl ester. By "protein" is meant a protein that
targets the emulsion to a specific cell type. A preferred
protein is an apoprotein, where the apoprotein may be free
of lipid or may be complexed covalently or ionically with
lipid to form an apolipoprotein.

30

In formulating the emulsions of the invention,
the charged lipid and hydrophilic biologically active
molecule are first mixed together in a charged lipid:
bioactive molecule ratio suitable to result in the
formation of a hydrophobic charged lipid:bioactive
35 molecule complex (herein "hydrophobic complex") which is

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soluble in the organic phase of a two phase aqueous-organic system. This hydrophobic complex is then mixed with triglyceride, cholesterol, phospholipid and optionally, cholesteryl ester, and/or apoprotein, to form the emulsions of the invention.

5 In a preferred embodiment, at least one negatively charged bioactive molecule is mixed together with at least one cationic lipid to form the hydrophobic complex.

10 In an alternative embodiment at least one positively charged bioactive molecule may be mixed together with at least one anionic lipid to form the hydrophobic complex.

15 By cationic lipid or anionic lipid is meant a lipid having a net positive (cationic lipid) or net negative (anionic lipid) charge at or near physiological pH.

20 It is believed that the emulsions of the present invention therefore comprise an apolar core composed of triglycerides and optionally, cholesteryl esters, into which the hydrophobic complex of a hydrophilic bioactive molecule and preferably, a cationic lipid, is incorporated; the apolar core being surrounded by a phospholipid monolayer in which cholesterol and optionally, specific apoprotein(s) are incorporated.

25 The invention also relates to methods of producing the emulsion formulations of the invention.

In one embodiment, the emulsion formulation of the invention may be produced by:

30 (a) mixing a hydrophobic complex of hydrophilic bioactive substance and cationic lipid with triglyceride, phospholipid, cholesterol and optionally cholesteryl ester in an organic solvent;

(b) removing the organic solvent to leave a lipid film;

35 (c) and suspending the film in an aqueous

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buffer to produce the emulsion.

If the emulsions are not uniform in size, the emulsions may be further purified to remove emulsions of undesired size. Such purification also serves to sterilize the emulsions.

In an alternative embodiment, where the emulsion formulation of the invention is to contain a water-soluble apoprotein, the apoprotein may be added to, and mixed with, the emulsion formed by the suspension of the film in step (c) above.

Of course, when isolated apoproteins such as apo-B-48 and apo-B-100, which are not soluble in aqueous buffer, are to be included in the emulsions, the above method of producing an emulsion containing apoproteins may be modified such that apoprotein is included among the components combined in the organic solvent prior to the film formation.

In an alternative embodiment, the emulsion formulations of the invention may be produced by dissolving the hydrophobic complex of cationic lipid and a hydrophilic bioactive molecule in the apolar core of a reconstituted lipoprotein emulsion.

In one embodiment, such a method comprises:

(a) extracting native lipoprotein, which preferably has been lyophilized, with an organic solvent;

(b) mixing the extracted lipoprotein lipids with a hydrophobic complex of cationic lipid and hydrophilic bioactive molecule in the organic solvent;

(c) removing the organic solvent to leave a lipid film;

(d) adding aqueous carrier to produce the emulsion; and

(e) purifying said emulsion, if necessary, to sterilize and obtain emulsions of desired size.

Typically, the emulsion formulations produced by this method would be apoprotein-free emulsions since most

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apoproteins are water-soluble and would not be contained in the organic solvent extract.

However, as noted above, apoproteins such as β -48 and β -100 are extractable with organic solvent. Therefore, it is understood that in cases where the lipoprotein to be extracted in step (a) is, for example, LDL, the organic extract to be mixed with hydrophobic complex in step (b) would contain apo-B-100 as well as the lipoprotein lipids. Of course, it is understood that even if the lipoprotein selected to be extracted by organic solvent does not contain apoprotein soluble in organic solvent, water-soluble apoprotein can be added to the aqueous suspension produced in step (d) in the above method to produce an apoprotein-containing emulsion.

In yet another embodiment, the emulsions of the invention may be produced by preparing the hydrophobic complex of cationic lipid and hydrophilic biologically active molecule as a dry film (i.e. by removal of the organic solvent into which the hydrophobic complex partitions), then adding native lipoproteins to the dry film and vortexing, such that the hydrophobic complex contained in the dry film rehydrates and partitions into the apolar core of the lipoprotein.

The invention therefore also relates to a lipid film capable of forming the emulsion formulations of the present invention upon suspension in an aqueous carrier. The film comprises triglyceride, cholesterol, phospholipid, cationic lipid, hydrophilic biologically active molecule and optionally, cholesteryl ester and/or water-insoluble apoproteins. Where the film comprises apoprotein, it is designated a lipid protein film.

The invention also relates to methods for delivering hydrophilic bioactive molecules to cells in vitro or in vivo.

In one embodiment, the method of delivering hydrophilic biologically active molecules to cells in vivo

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comprises administering to an animal an effective amount of an emulsion formulation of the present invention. Preferred animals are humans. Thus, for example, where the bioactive molecule is a gene or an oligonucleotide, the invention relates to the use of the emulsion formulations in gene or oligonucleotide therapies respectively.

Description of Figures

Figures 1A and 1B are cartoons showing proposed structures of an emulsion of the invention in which the hydrophobic DNA:TC-chol complex is incorporated into the apolar core of the emulsion.

Figure 2 shows the effect of various cationic lipids on the partitioning of ^{125}I -labelled DNA into the aqueous phase (top panel), organic phase (middle panel) or interphase (bottom panel) of a two phase system.

Figure 3 is a schematic showing the protocol for production of an emulsion of the invention by mixing a hydrophobic complex of DNA/ 3β [N', N', N' - trimethylaminoethane)-carbamoyl] cholesterol iodide (TC-chol) with olive oil, phosphatidylcholine, lysophosphatidylcholine, cholesteryl oleate and cholesterol.

Figures 4A and 4B show the distribution of ^{125}I -labelled DNA incorporated into emulsions as either DNA/TC-chol complex (Figure 4A) or free DNA (Figure 4B) following centrifugation. Fractions were collected from the top to the bottom and radioactivity was measured in a gamma counter.

Figures 5A and 5B present the distribution in a NaCl density gradient of either ^{125}I -labelled DNA incorporated into emulsions as ^{125}I -labelled DNA/TC-chol complex (Figure 5A) or of free ^{125}I -labelled DNA mixed with empty emulsions containing the same amount of TC-chol (Figure 5B). Density gradient fractions were collected

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from the top to the bottom of the tube and the radioactivity was measured in a gamma-counter.

Figure 6 illustrates the production of luciferase proteins in the indicated organs of mice following portal vein injection of either 100 μ g of naked DNA dissolved in hypertonic solution, 100 μ g of naked DNA dissolved in isotonic solution, or 100 μ g of DNA in the form of emulsions produced by mixing plasmid pCMVL DNA/TC-Chol complex with olive oil, phosphatidylcholine, lysophosphatidylcholine, cholesteryl oleate and cholesterol as described in Figure 3. The number of mice used in each experiment described in Figures 6-10 are indicated in parentheses in Figures 6-10 as n=___.

Figure 7 shows the production of luciferase proteins in the indicated organs of mice following tail vein injection of 100 μ g DNA in the form of either naked DNA or emulsions produced by mixing plasmid pCMVL DNA/TC-Chol complex with olive oil, phosphatidylcholine, lysophosphatidylcholine, cholesteryl oleate and cholesterol as described in Figure 3.

Figure 8 shows production of luciferase proteins in the indicated organs of mice following portal vein injection of 100 μ g of plasmid pCMVL DNA as the various formulations indicated in the Figure.

Figure 9 shows the production of luciferase proteins in the indicated organs of mice following portal vein injection of the indicated amounts of pCMVL DNA in the form of emulsions produced by mixing plasmid pCMVL DNA/TC-Chol complex with olive oil, phosphatidylcholine, lysophosphatidylcholine, cholesteryl oleate and cholesterol as described in Figure 3.

Figure 10 presents the results of a time course of luciferase protein expression in the indicated organs of mice following portal vein injection of 50 μ g of plasmid pCMVL DNA in the form of emulsions produced by mixing DNA/TC-Chol complex with olive oil,

phosphatidylcholine, lysophosphatidylcholine, cholesteryl oleate and cholesterol as described in Figure 3.

Figures 11A-11C show the effect of cationic lipids on the partition of DNA into organic phase.

¹²⁵I-DNA (4 µg) was incubated with indicated amounts of cationic lipids in the Bligh and Dyer monophasic (410 µl) at room temperature for 30 minutes. The monophasic was separated into two phases by the addition of chloroform and water (100 µl each). Partition of DNA into the aqueous phase (Figure 11A) and organic phase (Figure 11B) were determined by measuring their radioactivities. Partition of DNA into the interface (Figure 11C) was determined by subtracting the amount of DNA in the aqueous and organic phases from total DNA added. Each point presents the mean from three experiments ± s.d.

Figures 12A-D show the determination of DNA-incorporation into emulsions by centrifugation. DNA/TC-Chol complex (Figures 12A and 12C) or free DNA (Figures 12B and 12D) supplemented with a trace amount of ¹²⁵I-DNA was incorporated into emulsions (Figures 12A-C) or mixed with empty emulsions containing TC-Chol (Figure 12D). The samples (0.5 ml) were centrifuged in 4.5 ml (final) of water (Figures 12A and 12B) or NaCl density gradient (Figures 12C and 12D). Fractions (0.5 ml) were collected from the top to the bottom of centrifuge tubes and the radioactivities were measured.

Figure 13 shows gene expression in organs of mice following intraportal injection. CD1 mice were intraportally injected with 100 µg of plasmid pCMVL DNA in the various formulations. Two days after injection, mice were sacrificed and luciferase activity and protein concentration of tissue extracts were analyzed. Each column presents the mean from three animals ± s.d.

Figure 14 shows gene expression in organs of mice following intravenous injection. Mice were injected from the tail vein with naked pCMVL DNA or with pCMVL

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emulsions at the dose of 100 μ g of DNA. Two days after injection, mice were sacrificed and luciferase activity in the various organ extracts was measured. Each column presents the mean from three animals \pm s.d.

Figure 15 shows the dose dependence of gene expression by intraportal injection of various amounts of pCMVL emulsions into mice. Luciferase activity in the extracts from various organs was measured on day 2. Each column presents the mean from three animals \pm s.d.

Figure 16 shows the effect of pre-injection of empty emulsions on gene delivery by pCMVL emulsions. Fifteen minutes after intraportal injection of 0.6 ml of isotonic mannitol with or without empty emulsions (5.0 mg of total lipids), mice were intraportally injected with 50 μ g DNA of pCMVL emulsion dispersed in 0.6 ml of isotonic mannitol. Two days after injection, mice were sacrificed and luciferase activity in the various organ extracts was measured. Each column presents the mean from three animals \pm s.d.

Figure 17 shows the time course of gene expression after first and second injections. Mice were intraportally injected with 50 μ g DNA of pCMVL emulsions and sacrificed on the indicated day after injection. Some of them were injected again at day 7 by the same method as the first injection and were sacrificed 2 days after the second injection. Luciferase activity in the various organ extracts was measured. Each column presents the mean from three animals \pm s.d.

Figure 18 shows the delivery and expression of hAAT gene by emulsions. Mice were intraportally injected with 50 μ g DNA of pRSVhAAT emulsions or pAAVCMVhAAT emulsions. At the indicated days after injection, blood was collected from the tail vein of mice and serum concentration of hAAT was determined by ELISA. Each point presents the mean from three animals \pm s.d.

Figure 19 shows X-Gal staining of liver section

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0 from a mouse injected with pCMVLacZ emulsion. A mouse was
intraportally injected with 100 μ g DNA of pCMVLacZ
emulsion. Two days after injection, liver cryosections of
10 μ m in thickness were stained with X-Gal for 24 h.
After counter sections were examined under a light
5 microscope (Diaphot, Nikon) at an original magnification
of x 400.

Detailed Description of The Invention

10 This invention relates to emulsion formulations
designed to mimic native lipoprotein emulsions in vivo and
to the in use as vehicles for the delivery to cells of
hydrophilic biologically active molecules.

In particular, the emulsion formulations of the
invention comprise an aqueous carrier and the following
15 components: triglyceride, cholesterol, phospholipid, at
least one charged lipid which is preferably a cationic
lipid, at least one hydrophilic biologically active
molecule and optionally, cholesteryl ester and/or
apoprotein. It is contemplated that the inclusion of
20 apoproteins in the emulsion formulations of the inventions
is optional since apoprotein-free emulsions have been
demonstrated to complex with the appropriate apoproteins
in the circulation (Redgrave, T.G. and Maranhao, R.C.
(1985) Biochem. Biophys. Acta., 835:104-112) and still
25 target to receptor-bearing cells.

To produce the emulsions of the invention, the
charged lipid, which is preferably a cationic lipid, and a
hydrophobic biologically active molecule, which is
preferably negatively charged, are first mixed together to
30 form a hydrophobic complex which is soluble in the organic
phase of a two phase system. This hydrophobic complex is
then mixed with other lipid components which include
triglycerides, cholesterol, phospholipid, and optionally
cholesteryl ester. Apoprotein(s) may also optionally be
35 combined with the other lipids to produce the emulsion

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formulations of the invention.

The hydrophobic complexes to be mixed with the other lipid components and optionally, apoprotein, to produce the emulsion formulations of the invention, are produced by mixing charged lipid and hydrophilic bioactive molecule in a ratio that produces a complex soluble in an organic solvent such as chloroform.

It is understood that since the extraction efficiency approaches 100% when the charge ratio of cationic lipid to negatively charged bioactive molecule is about 1.0, the amount of cationic lipid to be mixed with a hydrophilic bioactive substance to form a hydrophobic complex may be readily determined by titrating increasing amounts of cationic lipid against a fixed amount of bioactive molecule at an appropriate pH and measuring the partitioning of the resultant complex into the organic phase of a two phase system. The pH and ionic strength of the system should be sufficiently controlled to allow for complex formation between the biologically active molecule and the charged lipid. Aqueous phases having low ionic strength are preferred. Thus, water is preferred over saline. Methods for measuring partitioning of the hydrophobic complex of cationic lipid and hydrophilic biologically active molecule into the organic phase include, but are not limited to, radiolabelling of the bioactive molecule as described in Example 1.

Cationic lipids suitable for complexing with hydrophilic bioactive molecules to produce a hydrophobic complex are any cationic lipid, or mixture of cationic lipids, which is capable of forming a complex that partitions into the organic phase of a two-phase aqueous/organic system. It is therefore contemplated that both monovalent and polyvalent cationic lipids may be utilized to form hydrophobic complexes with bioactive molecules. Preferred cationic lipids for use in forming the complexes of the invention include, but are not

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limited to, TC-Chol, and those cationic lipids referred to in Reimer et al. (Biochemistry (1995) 34:12877-12883) such as dimethyldioctadecylaminonium bromide (DDAB), dioleyldimethylammonium chloride (DODAC), 1,2-dioleoyl-3-N,N,N-trimethylaminopropane chloride (DOTMA) 2, 3-dioleoyloxy-N- [2-(spermidine carboxyamido) ethyl]-N,N-dimethyl-1-propaninium trifluoroacetate (DOSPA), diheptadecylamidoglycylspermidine (DHGS) and 1,2 bis (oleoyloxy)-3-(trimethylammonio) propane (DOTAP).

Preferred nmol/ μ g ratios of cationic lipid to bioactive molecule are those that result in recovery of at least 90% of the bioactive molecule in the organic phase, more preferably greater than 95% recovery in the organic and most preferably 100% recovery in the organic phase.

Examples of hydrophilic biologically active molecules which may be complexed with cationic lipid to form hydrophobic complexes include, but are not limited to, nucleic acids such as DNA, cDNA, RNA (full length mRNA, ribozymes, antisense RNA, decoys), oligodeoxynucleotides (phosphodiester, phosphothioates, phosphoramidites, and all other chemical modifications), oligonucleotide (phosphodiester, etc.) or linear and closed circular plasmid DNA; carbohydrates; proteins and peptides, including recombinant proteins such as for example cytokines (eg interleukins), trophic and growth or maturation factors (eg NGF, G-CSF, GM-CSF), enzymes, vaccines (eg HBsAg, gp120); and hydrophilic drugs. It is contemplated that when hydrophilic biologically active molecules are to be complexed with cationic lipid, one or more of the different bioactive molecules recited above may be included in the hydrophobic complex (eg, antisense oligonucleotides to two different genes).

Since the hydrophilic substance is believed to form a hydrophobic complex with the charged lipid based on charge interaction and the preferred charged lipid is a cationic lipid, preferred hydrophilic biologically active

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° molecules are negatively charged molecules such as nucleic acids, negatively charged proteins and carbohydrates including polysaccharides, or negatively charged drugs.

In a more preferred embodiment the biologically active molecules are nucleic acids and in a most preferred
5 embodiment, the nucleic acids are nucleic acids which encode a gene or a gene fragment or which effect transcription and/or translation.

Of course, it is understood that positively charged hydrophilic biologically active molecules could
10 also be readily formulated into the emulsions of the invention by mixing the positively charged biologically active molecule with an anionic lipid to produce a hydrophobic complex which is soluble in organic solvent. As with the hydrophobic complex of cationic lipid and
15 negatively charged bioactive molecule, the hydrophobic complex between anionic lipid and positively charged bioactive molecule could then be mixed with triglycerides, cholesterol, phospholipid and optionally, cholesteryl ester and/or apoprotein(s) to produce the emulsions of the
20 invention.

Suitable anionic lipids for complexing with a positively charged hydrophobic bioactive molecule to produce a hydrophobic complex are any anionic lipid, or mixture of anionic lipids, which are capable of forming a
25 complex that partitions into the organic phase of a two-phase aqueous/organic system. Examples of such anionic lipids include, but are not limited to, phosphatidyl glycerol, phosphatidic acid or a similar phospholipid analog.

30 The other lipid components, triglyceride, cholesterol, phospholipid and optionally, cholesteryl ester, which may be mixed with the hydrophobic complex to produce the emulsion formulations of the invention are those found in the four major classes of lipoproteins:
35 chylomicron, very low density lipoproteins, (VLDL), low

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density lipoproteins (LDL) and high density lipoproteins (HDL).

Triglycerides which may be used to formulate the emulsions of the present invention include purified triglycerides of varying fatty acid composition or vegetable oils which contain as their major component, triglycerides of various fatty acid compositions. Preferred sources of triglycerides are animal and vegetable oils, in particular, oils which have been shown to be suitable for use in vivo such as soya bean oil, olive oil, cottonseed oil, sesame oil, and cod liver oil. Such oils may be used alone or in combination with other oils as a source of triglycerides. For example, olive oil and sesame oil may be used to formulate a single emulsion. A preferred oil is olive oil.

Phospholipid utilized to formulate the emulsion may be a single phospholipid species or a mixture of phospholipid species. Examples of phospholipids include, but are not limited to, phosphatidylcholine (PC), or phosphatidylethanolamine (PE), lyso PC or lyso PE, or fully saturated or partially hydrogenated PC or PE having aliphatic chains between about 6 and about 24 atoms in length.

By cholesteryl esters is meant cholesteryl esters containing saturated and unsaturated fatty acids of between about 10 and about 24 carbons in length esterified to the three carbon of cholesterol. Preferred cholesteryl esters are esters of unsaturated fatty acids between 16 and 18 carbon atoms in length such as oleic acid. It is contemplated that a single species of cholesteryl ester or multiple species of cholesteryl ester may be used in formulating an emulsion formulation of the invention.

When apoproteins are to be included in the emulsion of the invention, one or more of the different apoproteins may be selected from any of the apoproteins shown in Table 1.

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TABLE 1

Lipoprotein	Chylomicrons	VLDL	LDL	HDL
Major apoproteins	AI, AIV, B-48, CI, CII, CIII, E	B-100, CI, CII, CIII, E	B-100	AI, AII, E

The apoproteins to be utilized in the present invention may be isolated from native lipoproteins by known methods such as extraction of lipoproteins with organic solvent or detergents or they may be recombinantly expressed (examples of apoproteins which have been cloned include E, B-100 and AI) and then purified by methods known to those of ordinary skill in the art. Since it is contemplated that the addition of apoprotein to the emulsion formulation may produce an emulsion which demonstrates enhanced efficiency and specificity of delivery of the bioactive substance due to efficient receptor-mediated uptake of the apoprotein-containing emulsion formulation, preferred apoproteins to be included in the emulsions of the invention are those that are involved in receptor-mediated catabolism such as apo B-100 and apo E. For example, reconstituted chylomicrons appear to be taken up by hepatocytes via apolipoprotein E-specific receptors (Huettinger, M. et al., *Clin. Biochem.*, 21, 87-92 (1988); Rensen, P.C.N. et al. *B. Nat. Med.*, 1, 221-225 (1995)).

It is further contemplated that when apoproteins are included in the emulsion formulations of the invention, the apoproteins may be modified to direct the emulsion formulation to non-lipoprotein receptors. For example, reductive lactosamination of LDL and HDL has been demonstrated to direct these lipoproteins to galactose receptors present on Kupfer cells and liver parenchymal cells (Bijsterborch, M.K. and van Berkel, Th. J.C. (1992) *Anol. Pharmacol.* 41:404-411) and acetylation of LDL

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directs that lipoprotein to macrophages, monocytes and endothelial cells (Shaw, J.M. (1991), et al., Lipoproteins are Carriers of Pharmacological Agents", Marcel & Dekker, NY, NY.)

In addition, the apoproteins may be chemically modified with, for example, monoclonal antibodies exhibiting specificity towards cell-surface components, in order to broaden the range of cellular specificities of the emulsion formulations of the invention. (see Shaw, J.M. ed. (1991) "Lipoproteins as Carriers of Pharmaceutical Agent"; Marcel Dekker Inc. NY, NY).

The weight ratios of triglyceride, cholesterol and phospholipid and optionally cholesteryl ester, to be mixed with the hydrophobic complex to form the emulsions of the invention may be selected from the ranges of the weight percentages of these four lipid components known to be found in chylomicrons, VLDL, LDL and HDL as shown below in Table 2.

TABLE 2

Lipoprotein	Chyomicrons	VLDL	LDL	HDL
Phospholipids (%)	3-6	15-20	18-24	26-32
Cholesterol (%)	1-3	4-8	6-8	3-5
Cholesteryl esters (%)	2-4	16-22	45-50	15-20
Triglycerides (%)	80-95	45-65	4-8	2-7

Thus, the dry weight % of phospholipids may range from about 3% to about 32%, the weight % of cholesterol may range from about 1% to about 8%, the weight % of cholesteryl esters may range from about 0% to about 50% and the weight % of triglycerides may range from about 2% to be about 95%. More preferred ranges are phospholipids, 20-30%, cholesterol, 1-4%; triglycerides, 30-80%; and cholesteryl esters, 2-20%. Most preferred

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percentages are phospholipids, 25%; cholesterol, 2%, triglycerides, 70% and cholesteryl esters, 3%. The dry weight % of phospholipids, triglycerides, cholesterol and optionally cholesteryl esters given above are the dry weight %s to be mixed with the hydrophobic complex to produce the emulsions of the invention. These weight %s are believed to be similar to the weight %s of these lipids present in the resultant emulsion.

When mixed with the other lipid components (triglyceride, cholesterol, cholesteryl ester, phospholipid), the weight % of apoprotein as a % of the combined dry weight for the other lipids may range from about 1-2% to up to about 45-55%.

The amount of hydrophobic complex to mix with the other lipid components, and optionally apoprotein, to produce the emulsions of the invention is determined by the ratio of the weight of bioactive molecule in the hydrophobic complex to the total weight of the other lipid components. A preferred weight ratio of bioactive substance to other lipid components (cholesterol, triglycerides, cholesteryl ester, and phospholipid) in the emulsion of the invention is preferably from about 1:50 to about 1:400, more preferably 1:100 to about 1:300 and most preferably from about 1:150 to about 1:250.

The present invention therefore relates to methods for making the emulsion formulations of the present invention.

In one embodiment, the method comprises:

- (a) mixing the hydrophobic complex of cationic lipid and hydrophilic bioactive molecule in an organic solvent with triglycerides;
- (b) removing the solvent to leave a lipid film;
- (c) suspending the lipid film in an aqueous carrier to form the emulsion; and
- (d) purifying the emulsion, if necessary to sterilize and obtain emulsions.

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Where the emulsion of the invention is to contain a water-soluble apoprotein, the apoprotein may be added to, and mixed with, the emulsion formed by resuspension of the film.

5 Where water-insoluble apoproteins such as apo β -48 and apo β -100 are to be included in the emulsions of the invention, the emulsions are produced by including the water-insoluble apoprotein among the components combined in the organic solvent prior to the film formation.

10 In addition to being made from commercially available lipids and optionally, isolated apoproteins, the emulsion formulations of the invention may be produced by extracting native lipoproteins with, for example, organic solvents or detergents, and then reconstituting the components (lipids and optionally, apoprotein) extracted
15 from the lipoprotein in the presence of the hydrophobic complex.

In one embodiment, an emulsion produced by this approach is generated by:

- 20 (a) extracting native lipoprotein, which has preferably been lyophilized, with an organic solvent;
- (b) incubating the extracted lipoprotein lipids with the hydrophobic complex of cationic lipid and hydrophilic bioactive molecule;
- (c) removing the solvent to leave a lipid film;
- 25 (d) suspending the lipid film in an aqueous carrier to produce the emulsion; and
- (e) purifying the emulsion, if necessary to obtain emulsions of defined size and to sterilize the emulsion.

30 In this embodiment, the lipoprotein, which is extracted with organic solvent, is a native lipoprotein such as chylomicron, VLDL, LDL or HDL isolated from sera by methods known in the art such as density-gradient centrifugation, gel filtration, agarose gel
35 electrophoresis or plasmapheresis. Since most apoproteins

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° found in native lipoproteins are not extractable with organic solvent, most of the emulsions produced by the above method will be apoprotein-free emulsions unless 1) water-soluble apoprotein (either from the native lipoprotein or recombinantly produced) is added to the aqueous suspension produced in step (d) or 2) the lipoprotein contains an apoprotein which is extractable with organic solvent (eg. apo B-100 in LDL) such that the organic extract mixed with hydrophobic complex in step (b) will contain both lipoprotein lipids and organic-extractable (lipid-soluble) apoprotein.

The organic solvent used in the above methods may be any organic solvent which does not leave a toxic residue following removal and which solubilizes the lipid components of the emulsion. Examples of suitable solvents include lower alcohols, dimethoxyethane, dioxane, tetrahydrofuran, tetrahydropyran, diethylether, acetone, dimethylsulfoxide (DMSO), dimethylformamides (DMF), and halogenated hydrocarbons, such as chloroform, acetonitrile, or mixtures thereof. A preferred organic solvent is chloroform.

The organic solvent may be removed in the above methods under a suitable gas such as argon or nitrogen and/or under a vacuum. The dried film may then be lyophilized and stored at about -80 to about 37°C or may be resuspended in a suitable aqueous carrier. It is also contemplated that after the film is resuspended in an aqueous carrier, the resultant emulsion may be lyophilized and stored at about -80°C to about 37°C.

Aqueous carriers suitable for use in this invention, are non-toxic to cells and may or may not be buffered. When the carriers are buffered, suitable buffers include buffers such as citrate, carbonate, bicarbonate, acetate, Tris, glycinate and maleate. Aqueous carriers which may be used in the formulations of this invention include, but are not limited to, distilled

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water, normal saline solution and phosphate-buffered saline. It is understood that the aqueous carrier in which the film is suspended may include ingredients such as stabilizers, antibiotics, or antifungal and antimycotic agents.

"Purification" of the emulsions of the invention, where desired, may be carried out by density gradient centrifugation, gel filtration, FPLC or HPLC, or extrusion through membranes of a particular pore size. This purification step is preferred in the production of the emulsion formulations of the invention because it reduces the size of the emulsions to a uniform, small size by removing aggregates and it also serves to sterilize the emulsions.

Since the permeability of capillary endothelium to lipoproteins is known to vary widely among different tissues and may affect the rate of uptake by certain organs, the emulsions of the invention are preferably small enough to penetrate the smallest diameter fenestrations of endothelial cells. In a preferred embodiment, the average diameter of the emulsions of the invention is about 500 nm, more preferably about 200 nm and most preferably about 100 nm. It is contemplated that by altering the ratios of the various lipid components to mimic those found in more dense lipoproteins such as LDL or HDL or, by increasing the dry weight % of phospholipid, relative to the combined dry weight % of triglyceride, cholesterol and optionally cholesteryl ester, the diameter of the emulsion of the invention may be reduced.

The emulsions of the present invention may be utilized to deliver hydrophilic biologically active substances to cells in vitro or in vivo.

When the biologically active molecule is an antigenic protein or peptide, the emulsion formulations of the present invention may be utilized as vaccines.

In another embodiment, where the biologically

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active molecule is a polynucleotide such as a gene (a nucleic acid molecule comprising expression control sequences operatively linked to a nucleic acid sequence encoding a protein or peptide), it is contemplated that the emulsion formulations of the invention may be utilized to deliver genes to cells to treat or prevent disease. For example, the emulsions and methods of this invention may be used to deliver genes to hepatocytes to treat acquired diseases such as viral hepatitis infection (eg hepatitis B and C), cancer and alcoholic cirrhosis or to treat inherited diseases such as alpha 1-antitrypsin deficiency, familial hypercholesterolemia hemophilia A, tyrosinemia or phenylketonuria; to vascular endothelial cells to treat acquired diseases such as atherosclerosis and to reticuloendothelial cells to treat acquired diseases such as leishmaniasis.

In an alternative embodiment, where the polynucleotide is an oligonucleotide, the emulsion formulations may be used to treat acquired diseases such as viral infection or cancer.

Although the data presented herein demonstrates a high level of transgene expression when an emulsion resembling a chylomicron is used as the delivery vehicle, it is contemplated that since the receptors of other lipoproteins such as LDL and HDL are widespread among many cell-types, emulsions which mimic these lipoproteins in vivo may also be an efficient vehicle for delivery of hydrophobic bioactive molecules to target tissues other than the liver. Those of ordinary skill in the art will readily understand that the emulsion formulations of the invention may therefore be used to specifically deliver hydrophilic bioactive molecules to cells which express receptors specific for the apoprotein or other targeting protein(s) contained in the emulsion formulation as formulated or which is incorporated into the emulsion in vivo. For example, since the LDL receptor is found in

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cells such as hepatocytes, fibroblasts and endothelial cells, bioactive molecules could readily be delivered to these cells by emulsion formulations containing the apoprotein found in LDL.

Suitable routes of administration of the emulsion formulations of the invention to an animal include inoculation or injection by, for example, intravenous, oral, intraperitoneal, intramuscular, subcutaneous, intra-aural, intraarticular or intra-mammary routes, topical application, for example on the skin, scalp, ears or eyes and by absorption through epithelial or mucocutaneous linings, for example, nasal, oral, vaginal, rectal and gastrointestinal among others, and as an aerosol. Those of ordinary skill in the art would readily understand that the mode of administration may determine the sites in the organism to which the biologically active substance will be delivered and may effect the amount of the formulation to be administered.

All articles or patents referenced herein are hereby incorporated by reference. The following examples illustrate various aspects of the invention but are in no way intended to limit the scope thereof.

Examples

MATERIALS AND METHODS

Materials

Cholesterol (Chol), cholesteryl oleate (Chololeate), L- α -lysophosphatidylcholine (Lyso PC), olive oil and dimethyldioctadecylammonium bromide (DDAB) were obtained from Sigma. L- α -Phosphatidylcholine (PC) were from Avanti Polar Lipid, luciferase from Calbiochem and 5-bromo-4-chloro-3-indoyl- β -D-galactoside (X-Gal) from Gibco BRL. Luciferase assay system and Coomassie Plus Protein Assay Reagent were from Promega and Pierce, respectively. Calibrator 4 as a standard for hAAT and goat anti-hAAT were purchased from Incstar and Vectastain ABC kit was from Vector.

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Plasmids

Plasmids pCMVL and pCMVLacZ contain a fire fly luciferase gene and a bacterial β -galactosidase (β -Gal) gene, respectively, and both of them are driven by a human cytomegalovirus immediate early promoter. pRSVhAAT (Guo, Z.S. et al. (1996) Gene Therapy 3:802-810) contains a hAAT gene driven by Raus sarcoma virus promoter. pAAVCMVhAAT was reconstructed from pAAVlac.26 (Kaplitt, M.G. et al. (1994) Nature Genetics 8:148-154) and pRSVhAAT as follows: pAAVlac.26 was digested with XbaI followed by ligation with double stranded oligodeoxynucleotide (5'-CTAGACTCGAGT-3') to insert a XhoI site. After digestion of both plasmids by HindIII and XhoI, the 4510 bp fragment from pAAVlac.26 and the 1680 bp fragment from pRSVhAAT were isolated and ligated together. The resulting pAAVCMVhAAT contains two AAV inverted terminal repeat (ITR) sequences flanking the hAAT gene driven by the CMV promoter. These plasmids were amplified in DH5 α strain of *E. coli*, isolated by alkaline lysis and purified by cesium chloride gradient centrifugation (Sambrook, J. et al. (1989) Molecular Cloning: A Laboratory manual (Cold Spring Harbor Laboratory Press, Cold Spring Harbor, N.Y.).

Synthesis of cationic derivatives of cholesterol

3- β -[N-(N', N'-dimethylethane)-carbamoyl]cholesterol (DC-Chol), a tertiary ammonium derivative of Chol, was synthesized as described previously (Goo, X. and Huang, L. (1991) Biochem Biophys Res Commun. 179:280-285). 3- β -[N(N', N', N'-trimethylethane)carbamoyl]cholesterol (TC-Chol), a quaternary ammonium derivative of Chol, was synthesized by methylation of DC-Chol with iodomethane.

Intraportal injection

For Examples 4-7

Six week old female CD1 mice were anesthetized via inhalation of dimethyl ether and intramuscular injection of 1 mg of ketamine-HCl and then treated as

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follows: the livers of mice exposed through a ventral midline incision were injected over 30 seconds into the portal vein using a 1/8 inch needle with 30 gauge and 1 ml syringe with various amounts of emulsion formulation dissolved in 1 ml isotonic mannitol solution.

For Examples 4A, 6A, 7A 7B and 8

Six weeks old female CD1 mice were anesthetized with intramuscular injection of ketamine hydrochloride (1 mg/20 g of body weight). After the liver was exposed through a ventral midline incision, various amounts of DNA/TC-Chol-emulsion which was dispersed in 1 ml of 5.2 % (isotonic) mannitol, were injected into the portal vein using a 1/2 inch 30 gauge needle and 1 ml syringe.

X-Gal staining. Forty-eight hours after injection, the liver was perfused in situ with 5 ml of 1.25 mM EGTA in PBS (pH 7.5) to remove the blood. The liver was dissected, cut into small blocks and frozen in OCT embedding compound (Miles Scientific). Cryosections of 10 μ m in thickness were sampled and placed on polylysine-coated glass slides. Following fixation with 2 % glutaraldehyde in PBS containing 0.04 % Nonidet P-40, the liver sections were incubated in a staining solution (0.08 % 5-bromo-4-chloro-3-indolyl- β -D-galactoside (X-Gal), 5 mM each of $K_3Fe(CN)_6$ and $K_4Fe(CN)_6$ and 2 mM $MgCl_2$ in PBS) at 37°C for 24 h. The sections were then rinsed three times with PBS and lightly counter stained with hematoxylin.

ELISA for hAAT. ELISA method for measuring blood level of hAAT was modified from a published procedure (Kay, M.A. et al. (1995) Hepatology 21:815-819), except that an ABC kit containing avidin and biotinylated peroxidase was used.

Example 1

Solubilization of DNA in the organic phase

Since chylomicrons are emulsions containing no aqueous phase, native DNA cannot be incorporated into

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them. Accordingly, experiments were undertaken to "modify" the native DNA such that it would be hydrophobic and therefore be able to be incorporated into the chylomicron.

Four microgram of plasmid pCMVL DNA (plasmid pCMVL contains a luciferase gene driven by the human cytomegalovirus immediate early promoter) containing trace amounts of ^{125}I -labeled DNA was incubated with various nmol amount of 3β [N-(N',N'-dimethylaminoethane)-carbamoyl] cholesterol (DC-chol), DC-Chol:HCl, 3β [N', N', N' - trimethylaminoethane)-carbamoyl] cholesterol iodide (TC-chol) or dimethyldioctadecylammonium bromide (DDAB) in 410 μl of Bligh and Dyer monophasic (chloroform : methanol : water = 1:2.1:1, volume ratio) at room temperature for 30 minutes. Subsequently, the monophasic was partitioned into a two-phase system by the addition of 100 μl each of chloroform and water. The sample was then mixed by vortexing, and the separation of the upper aqueous and lower organic phases was facilitated by centrifugation at 600 x g for 5 minutes at room temperature. Two hundred microliters of the aqueous phase and 100 μl of organic phase were collected separately and their radioactivities were measured using a γ -counter. Radioactivity of the interface was calculated by subtracting the radioactivity of the aqueous and organic phases from the total radioactivity.

As shown in Figure 2, DC-chol did not change the solubility of DNA in the aqueous phase. It is believed this failure of DC-Chol to change the solubility of the DNA might be due to the cationic charge of DC-Chol not being strong enough to form a hydrophobic complex with DNA, perhaps due to incomplete ionization of DC-chol in the monophasic.

In addition, while the solubility of DNA in the aqueous phase was drastically decreased in the case of the hydrochloric acid salt of DC-chol, the resulting

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hydrophobic complex was not soluble in the organic phase but stayed at the interface.

However, when a quaternary ammonium derivative of DC-Chol, TC-Chol, was used to form a hydrophobic complex with DNA, it was observed that formation of hydrophobic complex in the interface was saturated at 20 nmoles of TC-chol (ie a ratio of cationic charge of TC-chol to anionic charge of DNA of about 1.8). Moreover, at concentrations of TC-Chol greater than 20 nmol, the complex in the interface was quantitatively transferred to the organic phase thereby suggesting that TC-Chol could form a hydrophobic complex with DNA that could be incorporated into emulsions. The results obtained with TC-chol were almost the same as that obtained from another cationic lipid having a quaternary amine, dimethyldioctadecyl-ammonium bromide (DDAB) (Figure 2).

Example 1A

Four μ g of plasmid DNA containing trace amount of 125 I-labeled DNA was incubated with various amount of cationic lipids in 410 μ l of Bligh and Dyer monophasic (chloroform: methanol: water = 1 : 2.1 : 1) at room temperature for 30 min. Subsequently, the monophasic was partitioned into a two-phase system by the addition of 100 μ l each of chloroform and water. The sample was mixed by vortexing, and the separation of the upper aqueous and lower organic phases was facilitated by centrifugation at 2,000 x g for 10 min at room temperature. Two hundred μ l of the aqueous phase and 100 μ l of the organic phase were collected separately and their radioactivities were measured using a gamma-counter (Gamma 5500B, Beckman). Radioactivity in the interface was calculated by subtracting the radioactivities of aqueous and organic phases from the total radioactivity. As shown in Figure 11A, the DC-Chol did not increase the solubility of DNA in the organic phase. Further, although DC-Chol hydrochloride, a salt form of DC-Chol, drastically

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decreased the solubility of DNA in the aqueous phase, the resulting hydrophobic complex was not soluble in the organic phase (Fig. 11B), but stayed at the interface (Fig. 11C). TC-Chol, a quaternary ammonium derivative of DC-Chol, formed a hydrophobic complex with DNA which is extractable with chloroform (Fig. 11B). At lower concentrations of TC-Chol, the amount of hydrophobic complex in the interface increased and reached the maximum level at 10 nmol of TC-Chol at which the ratio of cationic charge of TC-Chol to anionic charge of DNA was about 1 (Fig. 11C). After that, the complex in the interface (Fig. 1C) was quantitatively transferred to the organic phase (Fig. 11B). The results with TC-Chol were almost the same as that obtained with DDAB, a cationic lipid having a quaternary amine head group.

Example 2

Production of emulsions by mixing hydrophobic
PCMVL DNA/TC-Chol complex with olive oil,
phosphatidylcholine, lysophosphatidylcholine,
cholesteryl oleate and cholesterol

PCMVL DNA/TC-Chol complex corresponding to 200 μ g of DNA was prepared as described in Example 1 and was mixed with 40 mg of lipids (olive oil: L- α -phosphatidylcholine: L- α -lysophosphatidylcholine : cholesteryl oleate:cholesterol in a 70 : 22.7 : 2.3 : 3.0 : 2.0 weight ratio) dissolved in chloroform and evaporated under a stream of nitrogen to make a lipid film in a glass tube. Following vacuum desiccation for 1 hour, 1.6 ml of water was added and left at room temperature for 1 hour. The mixture of hydrated lipids and DNA-TC-chol complex was emulsified by vortexing for 2 minutes followed by homogenization for 30 seconds using a Tissue Tearor (Model 985-370, Biospec Product) at 65°C. Finally, the emulsions were extruded 20 times through a polycarbonate membrane with 100 nm pore size (see Figure 3). The resulting emulsions, designated emulsion formulation #1, were homogeneous particle populations with a mean diameter of

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106.9 \pm 16.2 nm (average \pm s.d., n = 3) as measured by light scattering using a submicron particle analyzer (Model N4SD, Coulter Electronics) and are utilized in Example 3-7.

Electrophoresis of emulsion formulation #1 on a 1% agarose gel, followed by staining with ethidium bromide, showed an absence of DNA degradation during incorporation of the hydrophobic DNA/TC-Chol complex into the emulsion.

Incorporation of the hydrophobic DNA/TC-Chol complex into emulsion formulation #1 was also confirmed by flotation as follows: the emulsion was diluted with water to a final volume of 4.5 ml and then centrifuged at 16,000 x g for 20 minutes at room temperature using an SW 50.1 rotor (Beckman). Half milliliter fractions were then collected from the top to the bottom of the tube and the radioactivity of ¹²⁵I-DNA in each fraction was measured. As shown in Figures 4A and 4B, more than 80% of DNA added as DNA/TC-Chol complex was floated up with the emulsions into three fractions from the top (Figure 4A) while when free DNA was used, no flotation of DNA was observed (Figure 4B). These results indicate that the hydrophobic DNA-TC-chol complex was almost completely incorporated or encapsulated into the emulsions.

Example 2A

Hydrophobic DNA/TC-Chol complexes prepared from 400 μ g of DNA and 1.25 mg of TC-Chol by the method described in Example 1A were incorporated into emulsions composed of olive oil : L- α -phosphatidylcholine: L- α -lysophosphatidylcholine : cholesteryl oleate:cholesterol (70 : 22.7 : 2.3 : 3.0 : 2.0, weight ratio) using the method described in Example 2. Emulsions produced by this method are utilized in Examples 3A, 4A, 5A, 6A, 7A, 7B and 8 and are designated as pCMVL, pLacZ, pRSVHAAT or pAAVCMVhAAT emulsions depending on the plasmid DNA used to formulate the emulsion.

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Incorporation of pCMVL DNA (in the form of hydrophobic complexes produced by the method described in Example 1A) into emulsions was determined by its flotation in centrifugation in the absence or presence of a density gradient. After extrusion, 0.5 ml of the emulsion was
5 mixed with 4 ml water and then centrifuged at 16,000 x g for 20 min at room temperature using a SW50.1 rotor (Beckman). In the case of the density gradient centrifugation, the emulsion (0.5 ml) was mixed with two-fold volume of NaCl solution with a density of 1.346
10 and discontinuous gradient was then formed using 1 ml each of NaCl solution with a density of 1.065, 1.020 and 1.006 (Redgrave, T.G. et al. (1985) Biochem. Biophys. Acts 835:104-112). Fractions of a half ml each were collected from the top to the bottom of the centrifuge tube and the
15 radioactivity of ¹²⁵I-DNA in each fraction was measured in a gamma counter. More than 65% of DNA added as the complex floated up with the emulsions into the top three fractions (Fig. 12A), whereas no flotation of DNA was observed when free DNA was used (Fig. 12B). This means
20 that more than two thirds of DNA/TC-Chol complexes were incorporated into the emulsions.

Example 3

Characterization of Emulsion Formulations

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Emulsion Formulation #1

Since it has been reported that hydrophobic complexes of cationic lipids and DNA are reversibly dissociated in the presence of NaCl at high concentrations
30 [Reimer, D.L., et al. *Biochemistry* 34, 12877-12883 (1995)], emulsion formulation #1, was mixed with two-fold volume of NaCl solution (d = 1.346), and then a discontinuous density gradient was formed using 1 ml each of NaCl solutions (d = 1.065, d = 1.020 and d = 1.006) and
35 centrifuged at 16,000 xg for 20 minutes at room

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temperature using an SW50.1 rotor.

As shown in Figure 5A, about 32% of ¹²⁵I-DNA was recovered in the emulsion fractions at the top of the tube. By comparison, when free DNA was mixed with empty emulsions containing the same amount of TC-chol and treated by density gradient centrifugation, no DNA was found in the emulsion fractions (Figure 5B).

Example 3A - pCMVL Emulsions

pCMVL emulsions were also mixed with NaCl solution and then density gradient centrifugation was carried out. About 32% of DNA was recovered from the upper emulsion fractions (Fig. 12C). When free DNA was mixed with empty emulsions containing TC-Chol in its lipid composition, the majority of DNA associated with the emulsion, resulting in flotation after the centrifugation in the water (data not shown). However, no flotation of DNA was observed after the NaCl density gradient centrifugation (Fig. 12D). Thus, at least 50% of DNA incorporated into emulsion is likely to be localized in the internal space of the emulsion. Resulting DNA/TC-Chol-emulsions had a homogeneous particle distribution with a mean diameter of 107 ± 16 nm (average \pm s.d., $n = 3$) measured by light scattering using a submicron particle analyzer (N4 Plus, Coulter Electronics).

Example 4

Animal Studies With Emulsion Formulations

Emulsion formulation #1

In order to evaluate whether the emulsion formulation #1 could act as an effective gene delivery system in vivo, mice were injected intraportally with either emulsion formulation (corresponding to 100 μ g pCMVL DNA) dissolved in 1 ml of isotonic mannitol solution, 100 μ g naked DNA dissolved in isotonic mannitol solution or

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100 µg naked DNA dissolved in hypertonic solution (15% mannitol, 0.9% NaCl).

Two days after injection, the mice were sacrificed and the liver, spleen, lung, kidney and heart were collected. Luciferase activity in Examples 4, 5, 6 and 7 was determined as follows: Organs were homogenized with lysis buffer (0.05% Triton X-100, 2mM EDTA, 0.1 M Tris, pH 7.8). After two cycles of freeze (liquid nitrogen)-thaw (at 30C), the homogenates were centrifuged at 14,000 rpm for 10 minutes at 4°C. Twenty microliter of the supernatant was mixed with 100 µl of Luciferase Assay System (Promega) and relative light unit (RLU) was measured with a Luminometer (AutoLumat LB953, EG&G, Berthold). Conversion from RLU to luciferase protein mass was calculated from a standard curve (0.01 to 1.0 ng; ng luciferase = (RLU + 1975.4)/3.5553 x 10⁴) based on purified luciferase protein standards (Sigma). Protein concentration was also determined by a Coomassie Plus Protein Assay Reagent (Pierce), using BSA as a standard.

As shown in Figure 6, high amounts of luciferase protein were produced in the livers of mice injected intraportally with the emulsions while the production of luciferase protein was almost 100-fold lower for injection of naked DNA in isotonic solution and 10-fold lower for infection of naked DNA-hypertonic injection solution (15% mannitol, 0.9% NaCl).

In addition, while luciferase protein was also produced in the spleen, lung and heart of mice injected with emulsion formulation #1, the level of expression was 25- to 800-fold less than the liver. In the case of naked DNA, substantial luciferase production was also found in the kidney. Finally, since total liver extract contained about 170 mg of protein, it appeared that more than 800 ng of luciferase protein was produced in the entire liver of the emulsion-injected mice.

By comparison, as shown in Figure 7, the level

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of luciferase protein produced in the liver of the mouse injected in the tail vein with emulsion formation #1 (corresponding to 100 μ g pCMVL DNA) was much lower than that observed in the livers of mice injected intraportally with emulsion formulation #1 (compare Figure 7 with Figure 6). However, as for the intraportally injected mice, the tail vein-injected mouse also showed greater luciferase production (about 6-fold) in the liver when injected with emulsions as compared to naked DNA (Figure 7). In addition, much higher production of luciferase protein was found in the kidney than in the liver in the case of injection of naked DNA (Figure 7).

In sum, higher gene expression was obtained when the emulsions were injected into the portal vein rather in the tail vein.

Example 4A-pCMVL Emulsions

Mice were injected intraportally with 100 μ g DNA of pCMVL emulsions produced as described in Example 2A and 2 days after injection, the mice were sacrificed and liver, spleen, lung, kidney and heart were collected. Luciferase activity for Examples 4A, 5A, 6A and 7A was determined as follows: Organs were homogenized with lysis buffer (0.05% Triton X-100, 2 mM EDTA, 0.1 M Tris, pH 7.8) using a Tissue Tearor for 1 min. After 2 cycles of freeze in liquid nitrogen and thaw at 37°C, the homogenates were centrifuged at 14,000 x g for 10 min at 4°C. Twenty μ l of the supernatant were mixed with 100 μ l of Luciferase Assay System and relative light unit (RLU) was measured with a luminometer (AutoLumant LB 953, EG&G) for 20 seconds. Conversion from RLU to luciferase protein mass was calculated from a standard curve (1 to 10,000 pg; pg luciferase = $-5.0 + 8.3 \times 10^{-3} \times \text{RLU}$, $r^2 = 0.99$) based on purified luciferase protein as a standard. Protein concentration of the supernatant was also determined by a Coomassie Protein Assay Reagent, using bovine serum albumin as a standard.

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As shown in Fig. 13, a high amount of luciferase protein was produced in the liver. The level was almost 100-fold higher than that of naked DNA-injected mice (Naked DNA, isotonic). Although the level of gene expression in the liver by naked DNA was significantly increased when a hypertonic solution (15% mannitol, 0.9% NaCl) was used for injection (Naked DNA, hypertonic) the level was still 10-fold lower than that of the pCMVL emulsions. Luciferase protein was also produced in the spleen, lung and heart by intraportal injection of pCMVL emulsions, but the levels were 25- to 800-fold less than that in the liver. The particle size of the pCMVL emulsions was important for an efficient gene delivery into hepatocytes. Injection of pCMVL emulsions without extrusion (pCMVL emulsion without extrusion) which had a mean diameter of 352 ± 135 nm, resulted in a low level of the luciferase protein production in the liver, spleen, lung and heart. The necessity of DNA incorporation into the interior of the emulsion was also examined by preparing empty emulsions with or without TC-Chol, and then mixed with 100 μ g of pCMVL DNA and injected. The emulsions containing TC-Chol formed aggregations immediately after the addition of DNA (TC-Chol-emulsion, DNA), and showed no gene expression in any organs. In the case of the mixture of DNA and empty emulsion without TC-Chol (emulsion, DNA), gene expression in each organ was almost the same as that of the mice injected with only naked DNA (Naked DNA, isotonic). These results indicate that high level of gene expression requires the location of DNA in the interior of the emulsion.

Example 5

In Vivo Gene Expression Following Portal Vein Injection Into Mice Of Naked pCMVL DNA Or Of Various Formulations Containing pCMVL DNA

One hundred micrograms of DNA in the form of naked DNA, emulsion formulation #1, emulsion formulation

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#1 without extrusion, empty emulsions containing TC-Chol and naked DNA, or empty emulsions without TC-Chol and naked DNA, were injected intraportally into mice and two days after injection, the mice were sacrificed and luciferase activity in various organs was assayed.

The results presented in Figure 8 show that as in Example 4 (see Figure 6), a high amount of luciferase protein was produced in the liver following injection of emulsion formulation #1 and the level was almost 100-fold higher than that observed for naked DNA.

Of interest, when emulsion formulation #1 without extrusion was injected, production of luciferase protein in the liver was low (Figure 8) (almost same as that in the spleen, lung and heart), suggesting that extrusion through a polycarbonate membrane with 100 nm pore size is necessary to prepare active reconstituted chylomicrons which are able to pass through fenestration of sinusoidal wall of liver and gain access to the hepatocytes. Moreover, TC-Chol-containing emulsions formed aggregations immediately after the addition of DNA, and did not show production of luciferase protein in any organs (Figure 8) while in the case of the mouse injected with naked DNA mixed with emulsions not containing TC-Chol, the production of luciferase protein in each organ was almost the same level as that of the mouse injected with only naked DNA (Figure 8).

Example 5A-pCMVL Emulsions

Distribution and strength of gene expression after tail vein injection was also examined in mice (Fig. 14) two days after injection of 100 μ g DNA of pCMVL emulsion. Gene expression is the highest in the liver and also in the lung and heart. The level of gene expression in the liver was significantly higher as compared with naked DNA, but was almost 100-fold lower than that of the mice injected intraportally (Fig. 14).

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Example 6Gene Expression In The Organs Of Mice
Following Portal Vein Injection With
Various Amounts Of Emulsion FormulationsEmulsion formulation #1

5 Mice injected intraportally with 0, 10, 25, 50, 75 or 100 μ g of DNA in the form of emulsion formulation #1 were sacrificed two days post-injection and luciferase activity in was assayed liver, spleen, lung, kidney, and heart.

10 As shown in Figure 9, production of luciferase protein in each organ increased with each increase in the injected dose and gene expression in the liver was almost saturated with injection of 50 μ g of DNA in the form of emulsion formulation #1.

Example 6A-pCMVL Emulsions

15 The effect of injected dose on the gene expression in mice following intraportal injection by pCMVL emulsion was also examined (Fig. 15). Even by injection of 10 μ g of DNA, pCMVL emulsion induced a measurable level of gene expression in the liver. The level of gene expression in each organ increased with increasing injected dose. In the liver, the gene expression jumped up between 25 and 50 μ g of DNA and was almost saturated with 100 μ g of DNA.

25 To reveal whether the gene expression in the liver results from uptake of emulsion particles themselves or not, the effect of empty emulsion pre-injection on the gene expression was investigated (Fig. 16). Gene expression in the liver by injection of 50 μ g DNA of pCMVL emulsions was reduced to about one-third by pre-injection of empty emulsion at the dose corresponding to 100 μ g DNA in pCMVL emulsions. However, the effect in the spleen and lung was opposite, i.e. three fold increase in the spleen and two fold increase in the lung. No effect was
35 observed in the kidney and heart.

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Example 7Time Course Of Gene Expression In Mice Injected
Intraportally With Various Emulsion FormulationsEmulsion Formulation #1

5 Fifty μ g of DNA was intraportally injected as
emulsion formulation #1 and the mice were sacrificed 1, 2,
3, 4, 5, 6 or 7 days after injection and luciferase
activity in liver, spleen, lung, kidney, and heart was
assayed.

10 As shown in Figure 10, gene expression reached
maximum level on day 2 except for the kidney and after day
2, the expression was gradually reduced and almost
disappeared on day 7 in the liver and kidney, and on day 4
in the spleen, lung and heart.

Example 7A-pCMVL Emulsions

15 Figure 17 shows the time course of gene
expression at the dose of 50 μ g of pCMVL DNA injected
intraportally. High level of gene expression was observed
at day 1 and day 2 in the liver, but there was a
20 significant reduction at day 3 (Fig. 17). After that,
gene expression in the liver gradually decreased and
almost disappeared by day 7. Other organs except the
kidney showed similar time course of change in gene
expression. The kidney retained a constant level of gene
25 expression from day 2 to day 6. Fig. 17 also shows the
possibility of repetitive injection of pCMVL emulsion
since two days after the second injection at day 7,
comparable gene expression to that obtained after the
first injection was observed in the liver.

Example 7B-PRSVhAAT and pAAVCMVhAAT Emulsions

30 Another time course experiment was carried out
using two different plasmids containing hAAT gene driven
by a different promoter (Fig. 18). In both cases,
significant amount of hAAT was produced and secreted into
the blood circulation. pAAVCMVhAAT, however, produced the
35 highest serum level (6 μ g/ml) of hAAT at day 2, which was

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17 fold higher than the highest serum hAAT level achieved at day 1 after injection of the same dose of pRSVhAAT. Moreover, although the serum level of hAAT rapidly decreased by 7 days after injection of both DNA, detectable concentration of hAAT was constantly observed until 60 days after injection of pAAVCMVhAAT (data not shown).

Example 8

Histochemical Analysis Of Gene Expression In The Liver

To elucidate the population and localization of cells in the liver which are transfected by intraportal injection of pCMVLacZ emulsions, pCMVLacZ DNA was complexed with TC-Chol and incorporated into emulsions (pCMVLacZ emulsion) as described in Example 2A and injected into a mouse. Liver cells expressing β -Gal activity were visualized by X-Gal staining (Fig. 19). Liver sections from a control (isotonic mannitol-injected) mouse or mouse injected with naked DNA did not show any change in color, while the color of liver sections from a mouse injected with pCMVLacZ emulsions turned to blue. By microscope examination of the liver cryosections from a control mouse, no β -Gal positive cell was observed (photo not shown). However, approximately 10 % of the cell population was stained by X-Gal and these blue cells were found all over the section. It appeared at higher magnification that these cells were not only hepatocytes, which have a polygonal shape and round nuclei, but also nonparenchymal cells (Fig. 19).

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Claims

1. A synthetic emulsion formulation comprising triglycerides, cholesterol, phospholipids, at least one charged lipid, at least one hydrophilic biologically active molecule and an aqueous carrier.
2. The emulsion formulation of claim 1, further comprising cholesteryl esters.
3. The emulsion formulation of claim 1, further comprising at least one apoprotein.
4. The emulsion formulation of claim 2, further comprising at least one apoprotein.
5. The emulsion formulations of claims 1-4, wherein the charged lipid is an anionic lipid and the hydrophilic biologically active molecule is positively charged.
6. The emulsion formulations of claims 1-4, wherein the charged lipid is a cationic lipid and the hydrophilic biologically active molecule is negatively charged.
7. The emulsion formulation of claim 6, wherein the hydrophilic biologically active molecule is a nucleic acid molecule.
8. The emulsion formulation of claim 7, wherein the nucleic acid molecule is a gene.
9. An emulsion formulation produced by
 - (a) mixing a hydrophobic complex of at least one charged lipid and at least one hydrophilic biologically active molecule with triglyceride,

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cholesterol and phospholipid in an organic solvent;
(b) removing said solvent to leave a lipid
film; and
(c) resuspending said film in aqueous
carrier to produce the emulsion formulation.

10. The emulsion formulation of claim 9,
wherein the weight ratio of biologically active molecule
to the sum of triglyceride, cholesterol and phospholipid
to be mixed in step (a) is about 1:50 to about 1:400.

11. The emulsion formulation of claim 9,
wherein the components of step (a) are further mixed with
cholesteryl esters.

12. The emulsion formulation of claim 11,
wherein the weight ratio of biologically active molecule
to the sum of triglyceride, cholesterol, cholesteryl
ester, and phospholipid in step (a) is about 1:50 to about
1:400.

13. The emulsion formulations of claims 9 or
11, wherein the components of step (a) are further mixed
with at least one water-insoluble apoprotein.

14. The emulsion formulations of claims 9 or
11, wherein the emulsion formulation produced in step (c)
is further mixed with at least one water-soluble
apoprotein.

15. A method of producing an emulsion
comprising: at least one charged lipid, at least one
hydrophilic biologically active molecule, triglyceride,
cholesterol, phospholipid and an aqueous carrier, said
method comprising:

(a) mixing a hydrophobic complex of

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charged lipid and hydrophilic biologically active molecule with triglyceride, cholesterol and phospholipid in an organic solvent;

(b) removing the organic solvent to leave a lipid film; and

(c) suspending said film in an aqueous buffer to produce the emulsion.

16. A method for producing an emulsion comprising at least one charged lipid, at least one hydrophilic biologically active molecule, triglyceride, cholesterol, phospholipid an aqueous carrier and optionally apoprotein, said method comprising:

(a) extracting native lipoprotein with an organic solvent;

(b) mixing the extracted lipoprotein components with a hydrophobic complex of charged lipid and hydrophilic biologically active molecule in an organic solvent;

(c) removing the organic solvent to produce a lipid or a lipid:protein film; and

(d) adding aqueous carrier to the film to produce the emulsion.

17. A lipid film capable of forming an emulsion formulation upon suspension in an aqueous carrier, said lipid film comprising triglyceride, cholesterol phospholipid, at least one charged lipid and at least one hydrophilic biologically active molecule.

18. The lipid film of claim 17, further comprising cholesteryl esters.

19. A lipid:protein film capable of forming an emulsion formulation upon suspension in an aqueous carrier, said film comprising triglyceride, cholesterol,

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° phospholipid, at least one charged lipid, at least one hydrophilic biologically active molecule, and at least one-water-insoluble apoprotein.

20. The lipid:protein film of claim 19, said
5 film further comprising cholesteryl esters.

21. A method of producing a lipid film having
at least one charged lipid, at least one hydrophilic
biologically active molecule, cholesterol, triglyceride
10 and phospholipid, said method comprising:

(a) mixing a hydrophobic complex of
charged lipid and hydrophilic biologically active molecule
with triglyceride, phospholipid and cholesterol in an
organic solvent; and

15 (b) removing said solvent to leave the
lipid film.

22. The method according to claim 21, wherein
the hydrophobic complex in step (a) is also mixed with
20 cholesteryl ester.

23. The method according to claim 21, wherein
the hydrophobic complex in step (a) is also mixed with at
least one apoprotein.

24. A method for delivering a hydrophilic
biologically active molecule to cells, said method
comprising exposing the cells to the emulsion formulations
of any one claims 1-3 thereby facilitating the delivery of
30 the biologically active molecule to the cells.

25. The method for delivering a biologically
active molecule to cells according to claim 24, wherein
the cells are exposed to the emulsion formulations in vivo
35 by administering the emulsion formulations to an animal in

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an amount effective to facilitate the delivery of the biologically active molecule to the cells of the animal.

26. The method of claim 25, wherein the biologically active molecule is a nucleic acid molecule.

27. The method of claim 24, wherein the cells are exposed to the emulsion formulations in vitro.

28. The method of claim 27, wherein the biologically active molecule is a nucleic acid molecule.

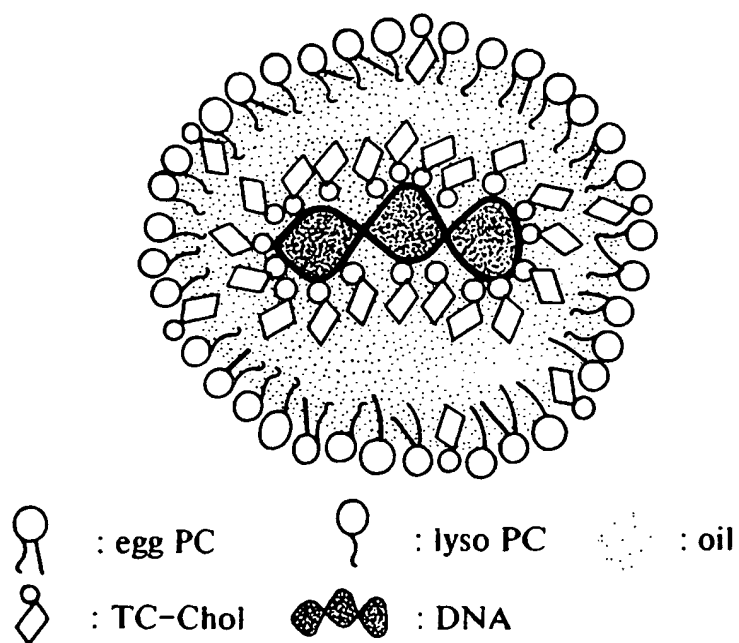


FIG. 1A

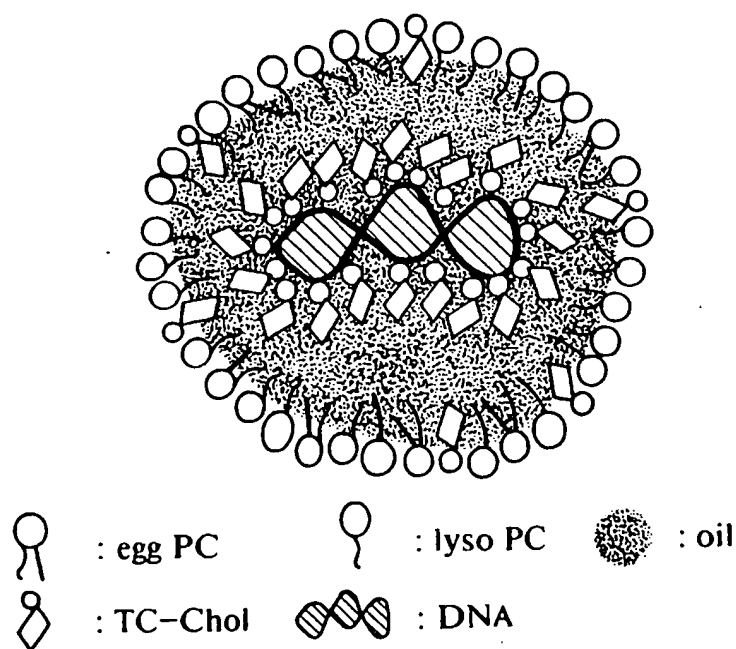


FIG. 1B

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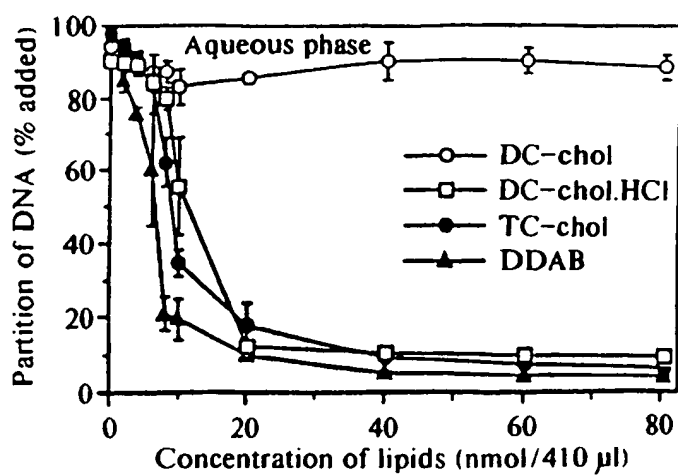


FIG. 2A

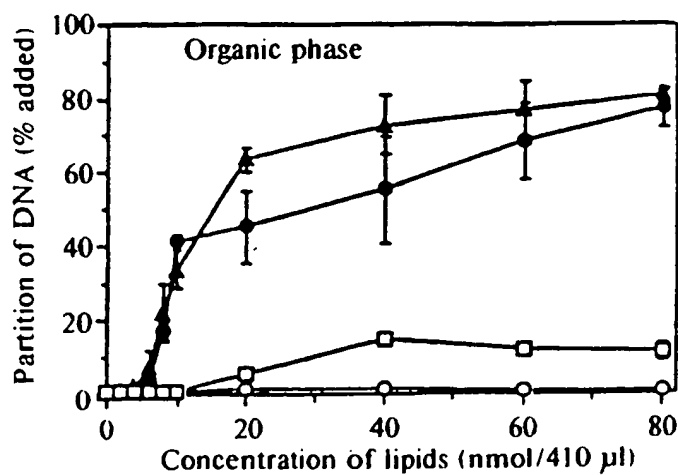


FIG. 2B

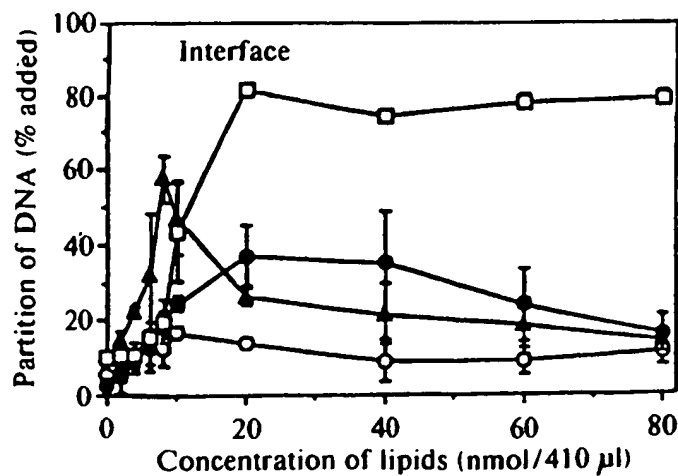


FIG. 2C

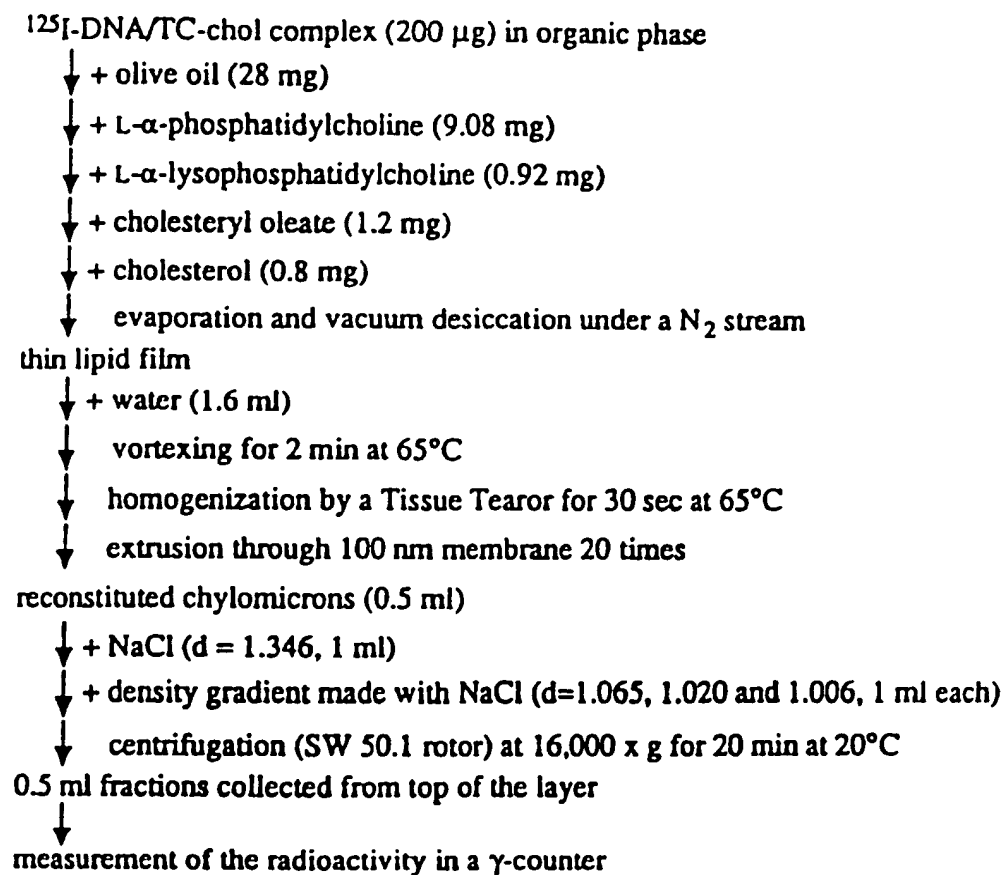


FIG. 3

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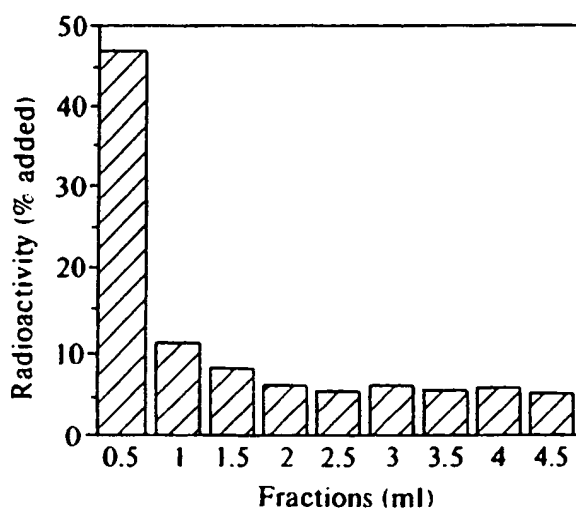


FIG. 4A

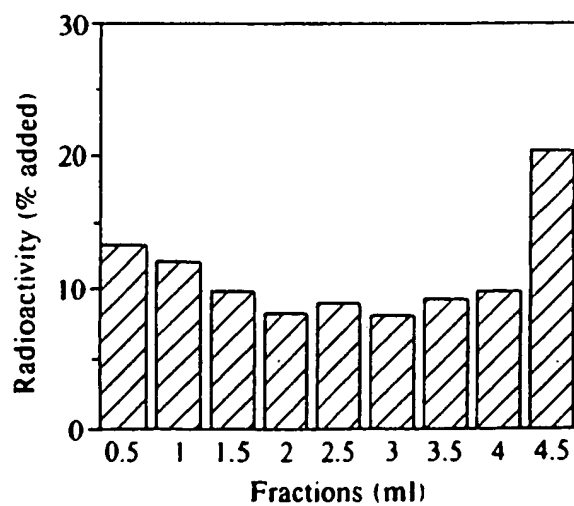


FIG. 4B

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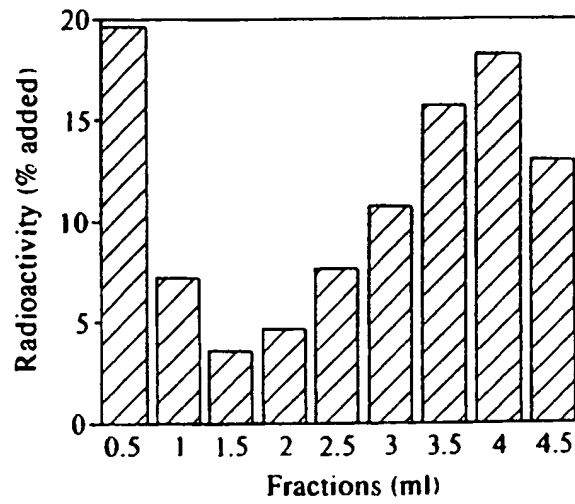


FIG. 5A

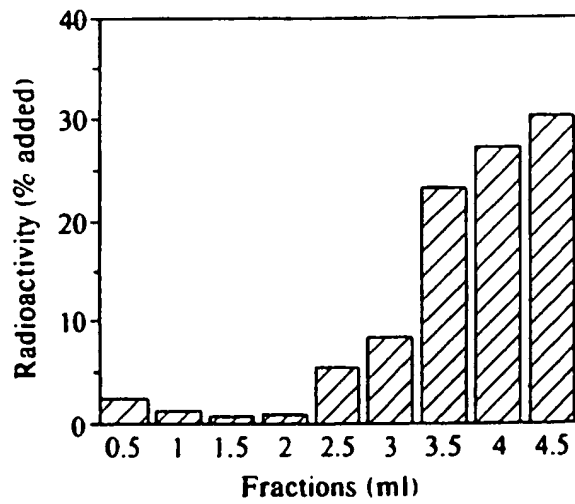


FIG. 5B

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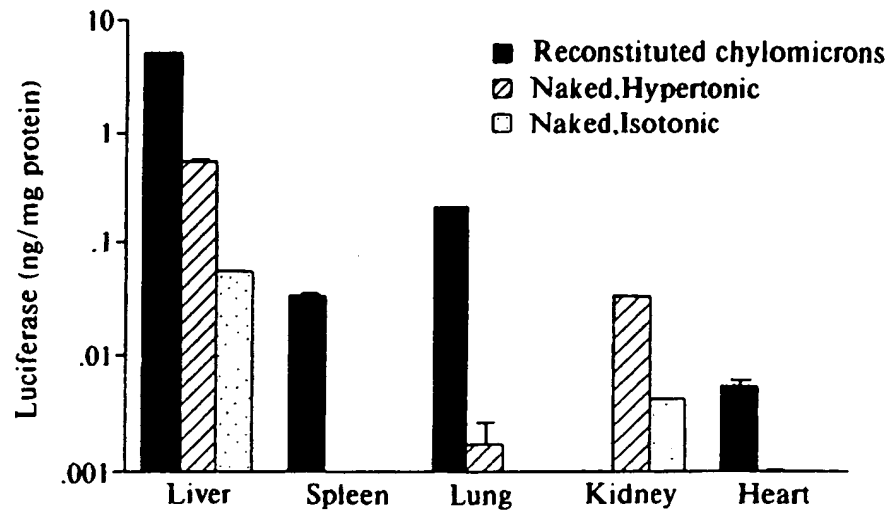


FIG. 6

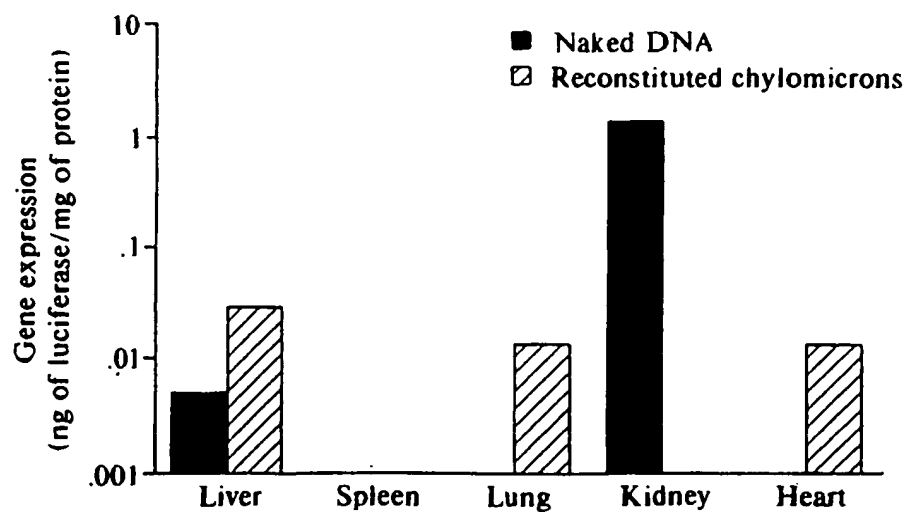


FIG. 7

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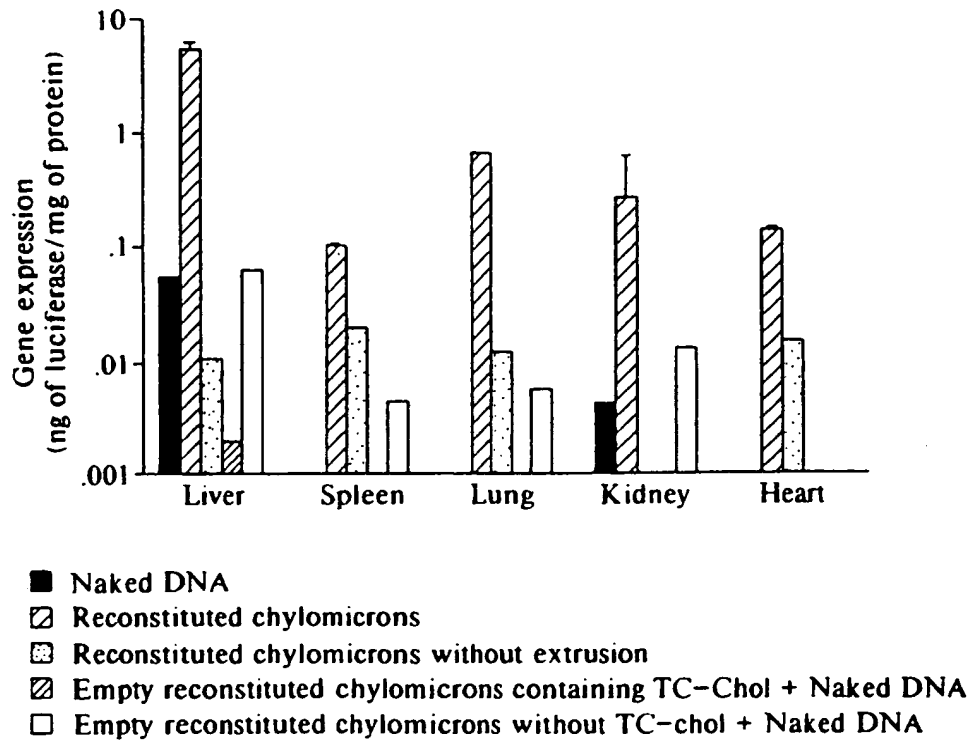


FIG. 8

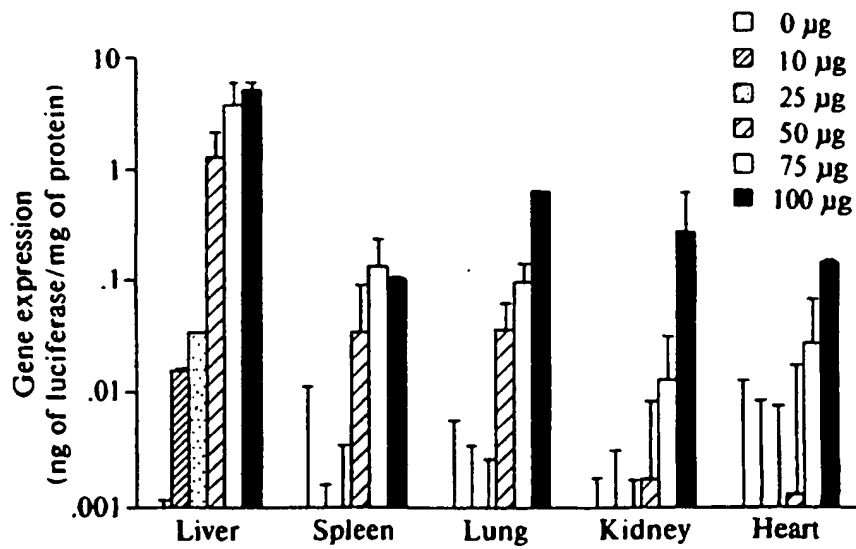


FIG. 9

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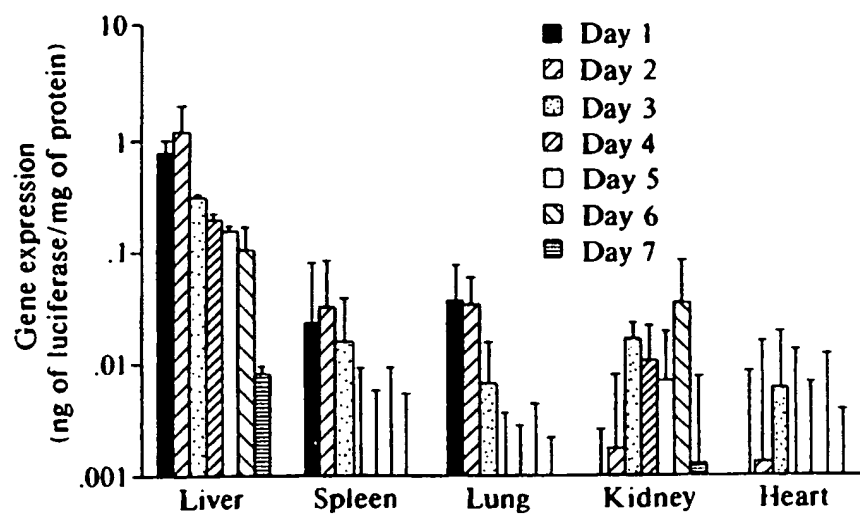


FIG. 10

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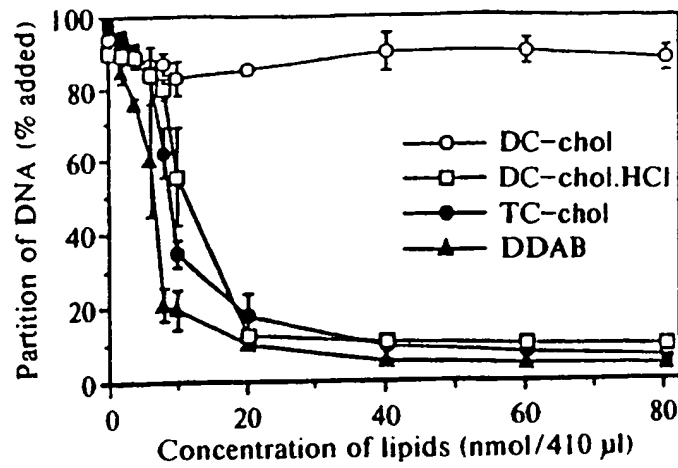


FIG. 11A

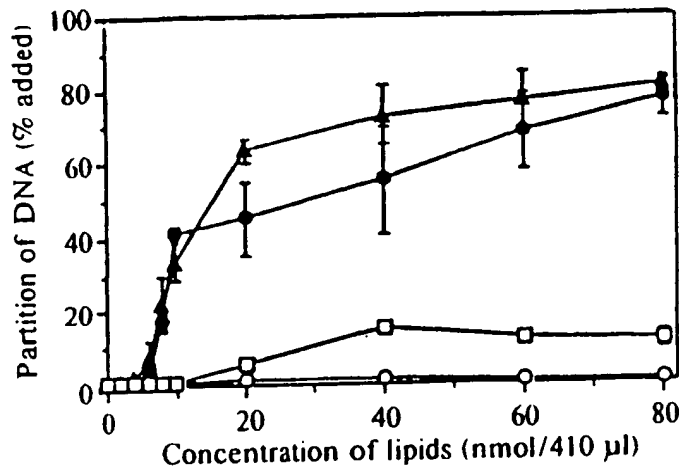


FIG. 11B

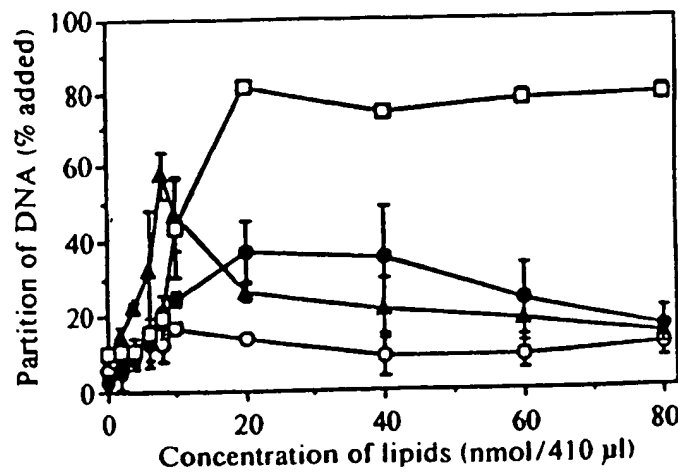


FIG. 11C

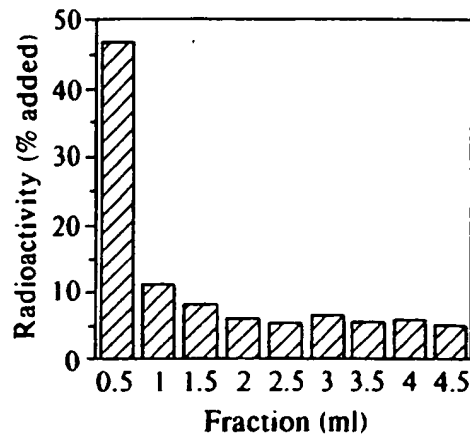


FIG. 12A

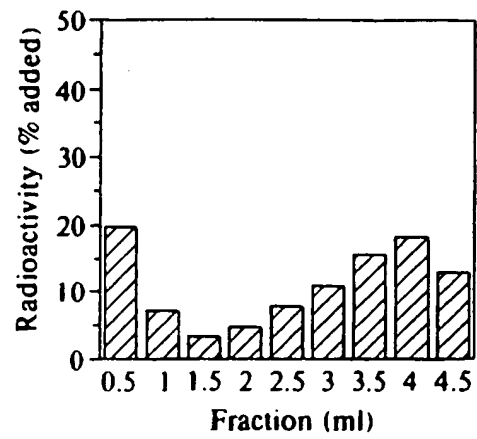


FIG. 12C

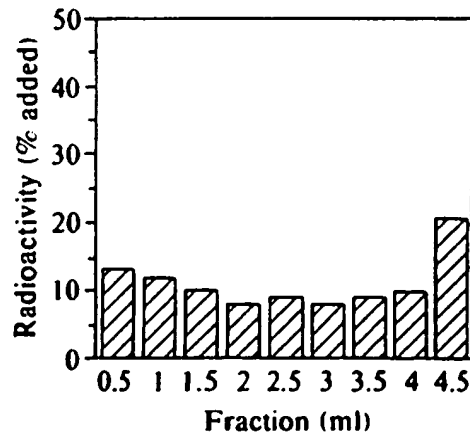


FIG. 12B

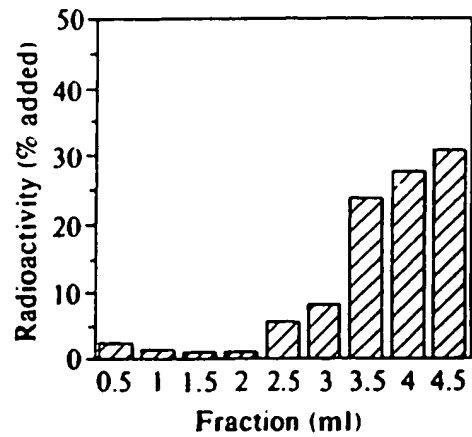


FIG. 12D

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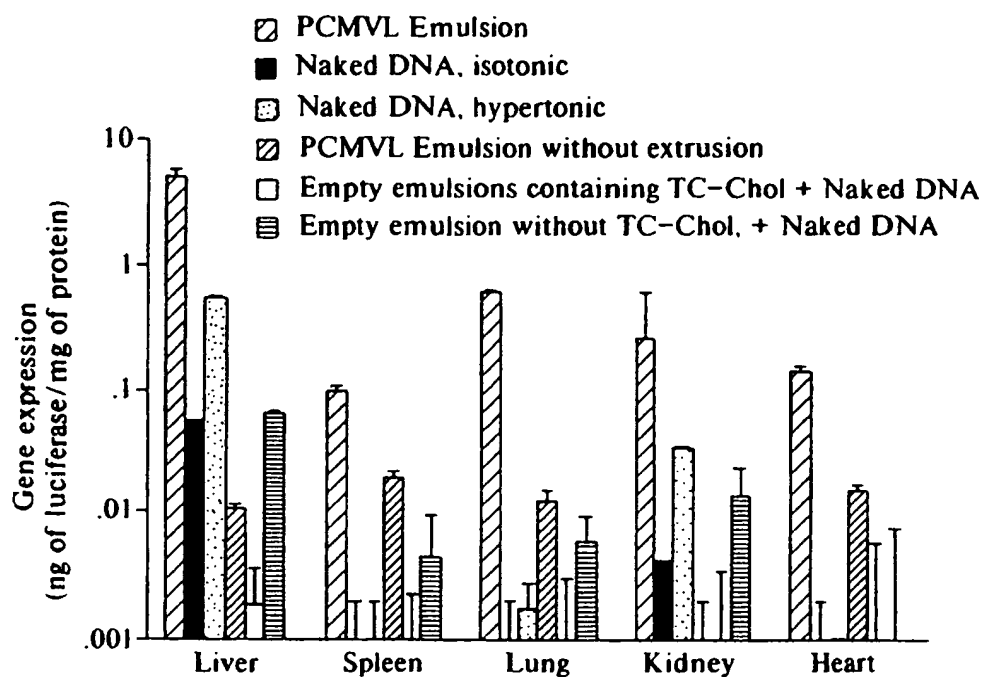


FIG. 13

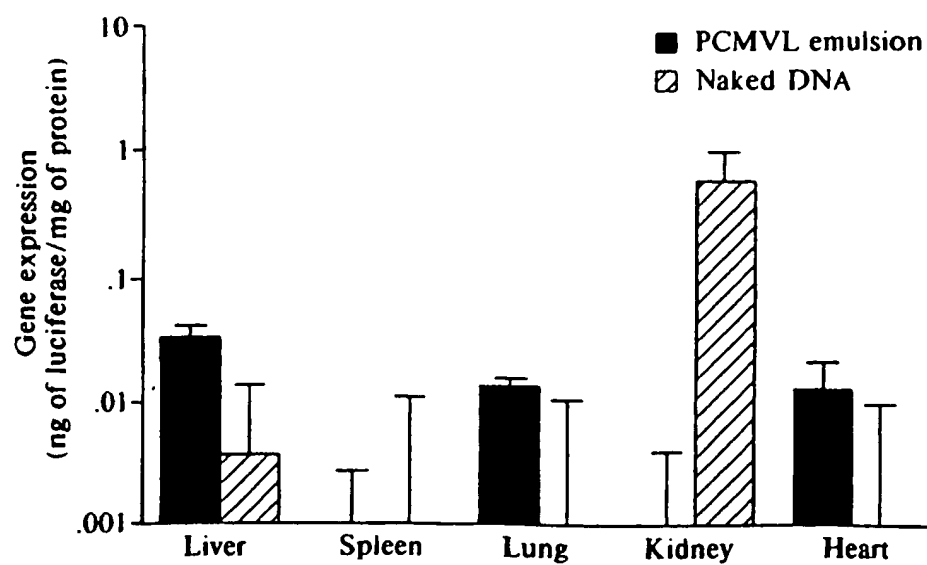


FIG. 14

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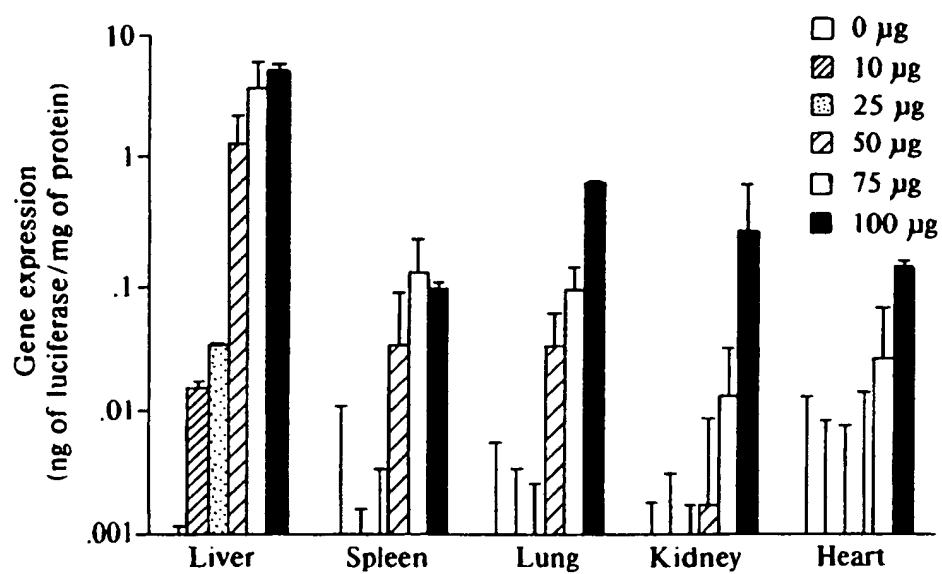


FIG. 15

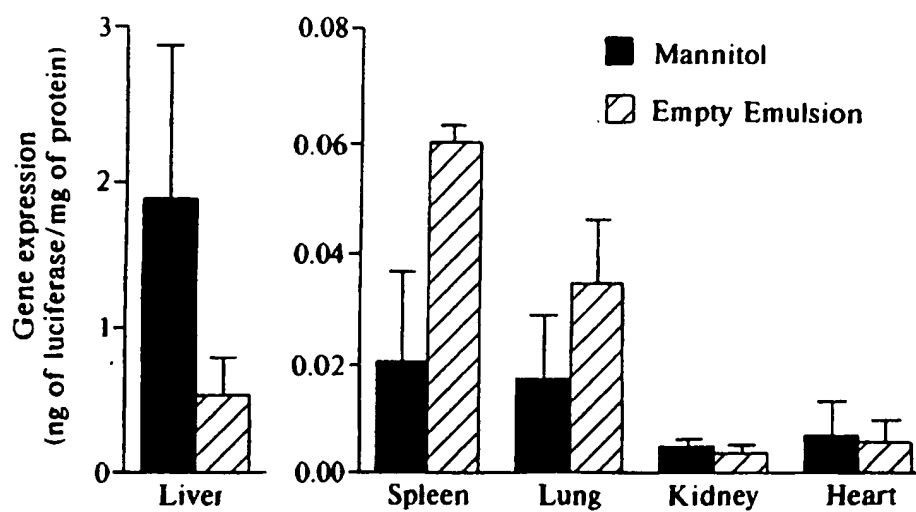


FIG. 16

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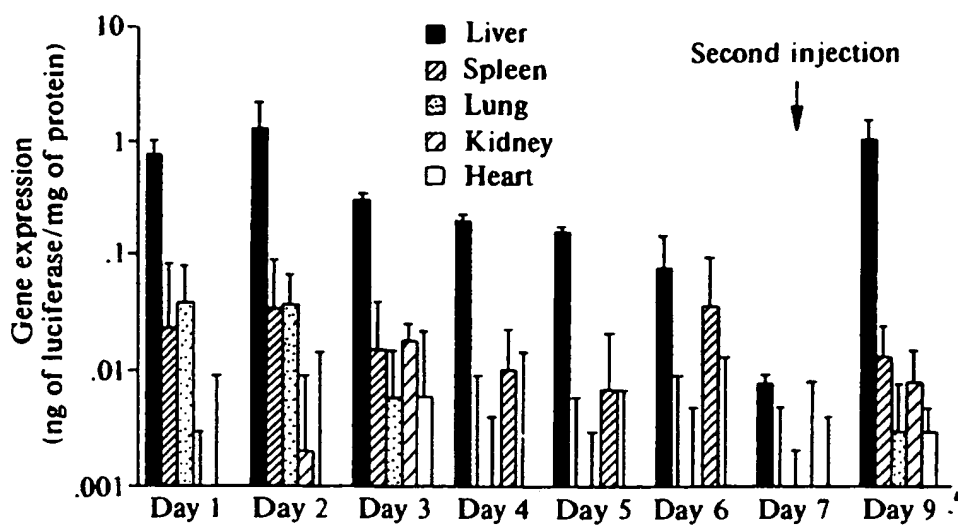


FIG. 17

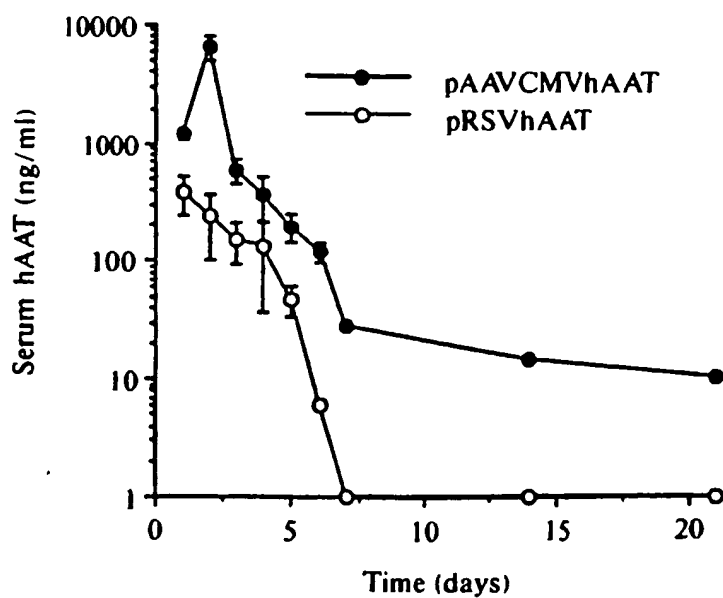


FIG. 18

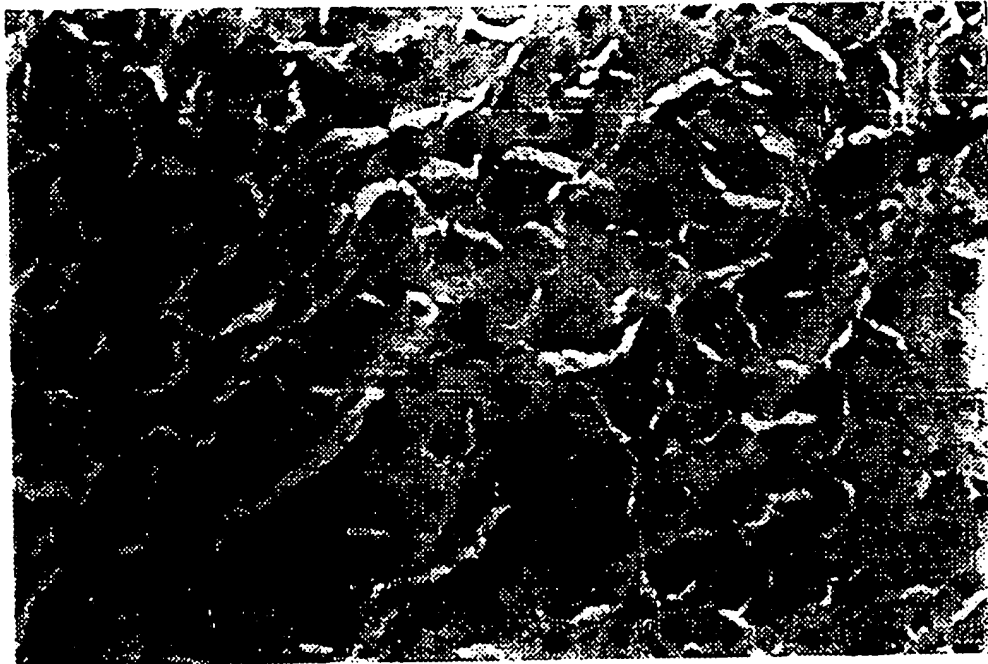


FIG. 19

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 97/12544

Box I Observations where certain claims were found unsearchable (Continuation of Item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.:
because they relate to subject matter not required to be searched by this Authority, namely:
Remark: Although claim(s) 25-26
is(are) directed to a method of treatment of the human/animal
body, the search has been carried out and based on the alleged
effects of the compound/composition.
2. ☐ Claims Nos.:
because they relate to parts of the International Application that do not comply with the prescribed requirements to such
an extent that no meaningful International Search can be carried out, specifically
3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a)

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all
searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment
of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report
covers only those claims for which fees were paid, specifically claims Nos..
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is
restricted to the invention first mentioned in the claims; it is covered by claims Nos.

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest
- ☐ No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

International Application No
PCT/US 97/12544

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	FR 2 649 321 A (INSTITUT NATIONAL DE LA SANTÉ ET DE LA RECHERCHE MÉDICALE) 11 January 1991 see page 7, line 8 - line 30 see page 9, line 1 - page 13, line 16 ---	9-15, 17-28
Y	A.-M. SAUTEREAU ET AL.: "physico-chemical characterization of low density lipoprotein containing a cytotoxic drug: the 2N-methyl-9-oleoyl-ellipticinium" EUROPEAN JOURNAL OF PHARMACEUTICS AND BIOPHARMACEUTICS, vol. 41, no. 2, April 1995, STUTTGART (DE), pages 136-139, XP000501189 see page 1, line 1 - page 2, column 1 ---	1-5, 9-12,15, 17,18, 21,22
Y	EP 0 387 647 A (DESITIN ARZNEIMITTEL GMBH) 19 September 1990 see the whole document see page 7; example 7 ---	1-5, 9-12,15, 17,18, 21,22
A	WO 93 05162 A (THE UNIVERSITY OF TENNESSEE RESEARCH CORPORATION) 18 March 1993 see the whole document -----	6-8

INTERNATIONAL SEARCH REPORT

Inter. Appl. No.
PCT/US 97/12544

A. CLASSIFICATION OF SUBJECT MATTER
IPC 6 A61K9/107 A61K48/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC 6 A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 90 03164 A (PATRALAN LIMITED) 5 April 1990	1-4
A	see page 5, line 5 - line 24 see page 12, line 1 - page 16, line 31 see page 47 - page 49; example 10 ---	16
X	WO 94 26252 A (PHARMIOS CORPORATION) 24 November 1994 see page 6, line 25 - line 34 see page 11, line 5 - line 22 see page 17, line 1 - page 18, line 26 see page 31, line 1 - line 12 ---	1-5
Y	see page 44; example 16 ---	9-15, 17-28
	-/--	



Further documents are listed in the continuation of box C.



Patent family members are listed in annex.

* Special categories of cited documents:

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- *L* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- *O* document referring to an oral disclosure, use, exhibition or other means
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- *T* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- *X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
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- *B* document member of the same patent family

Date of the actual completion of the international search

31 October 1997

Date of mailing of the international search report

11.11.97

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Fax: (+31-70) 340-3016

Authorized officer

Benz, K

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 97/12544

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
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